

Stent Technology 2009

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Memorial Regional Hospital

First Report of Coronary Stenting in 1987



The NEW ENGLAND
JOURNAL of MEDICINE

INTRAVASCULAR STENTS TO PREVENT OCCLUSION AND RESTENOSIS AFTER
TRANSLUMINAL ANGIOPLASTY

Ulrich Sigwart, M.D., Jacques Puel, M.D., Velimir Mirkovitch, M.D., Francis Joffre, M.D., and Lukas
Kappenberg, M.D.

N Engl J Med 1987; 316:701-6

Ulrich Sigwarth (Lausanne 1986)

First human coronary implantation

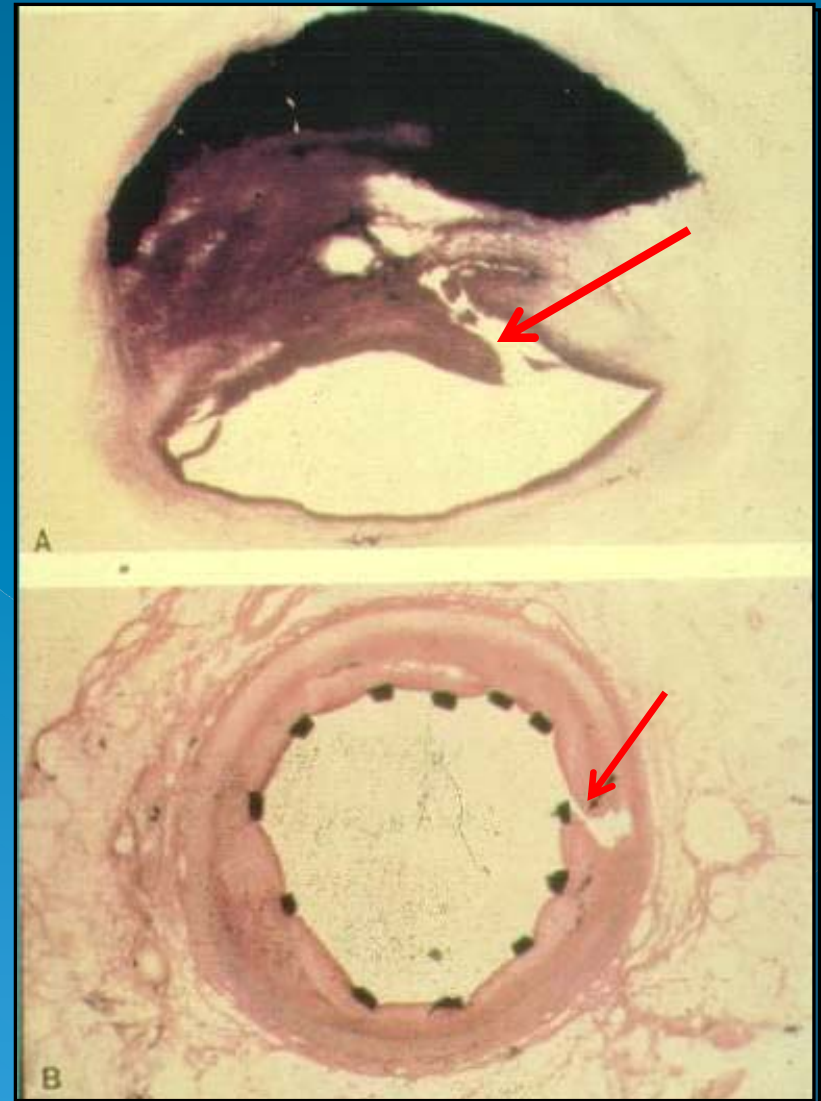
Expon

advances
ars



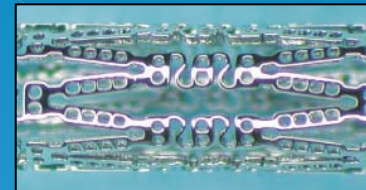
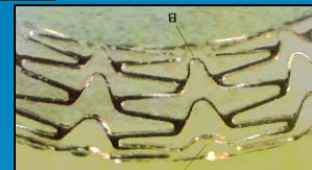
Why to Stent?

- Mechanically scaffold the artery and create a larger lumen predictably
- Prevent abrupt vessel closure
- Prevent restenosis



Stent Design

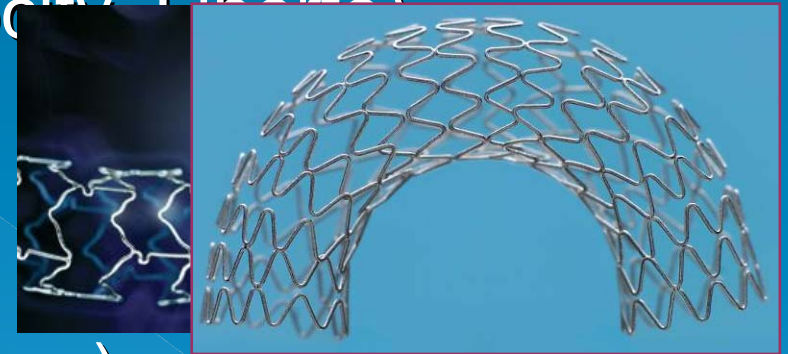
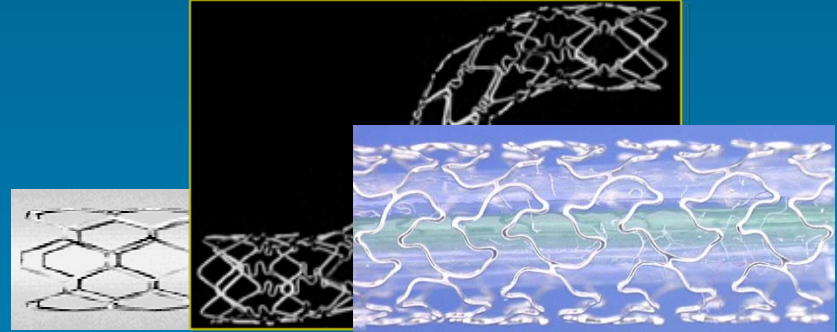
- Coil (Gianturco-Roubin)
- Slotted-tube (Palmaz-Schatz)
- Self-expanding mesh (Wallstent)
- multicellular or corrugated ring with flexible connections (majority of current stents)
- Open-cell or closed cell design



Features & Variables of Stent Design

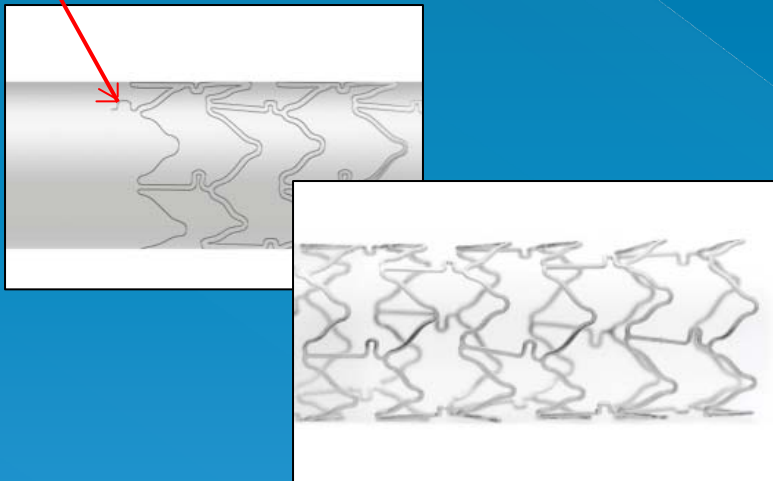
Strut material

- Stainless steel 316 L (Palmaz-Schatz, Velocity, Liberté)
- Tantalum (Wiktor)
- Nitinol (ACT-One)
- Cobalt chromium (Multilink VISION, Driver)
- Platinum chromium (Taxus & Promus Element)

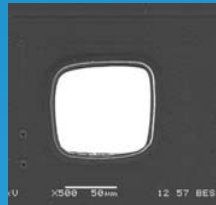


Basic strut types / Construction

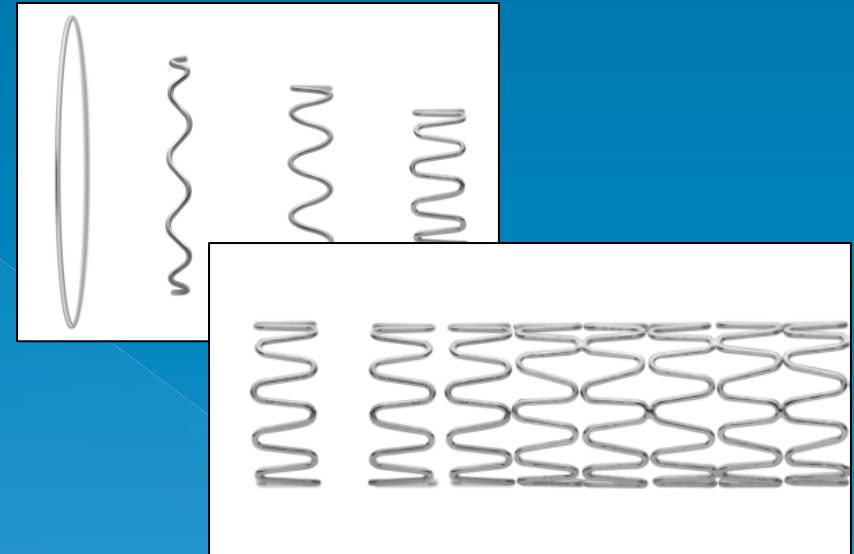
1. **Laser-cut struts** start as a tube, a laser removes material and a stent remains. Laser-cut stent production leaves square (blunt) edges.



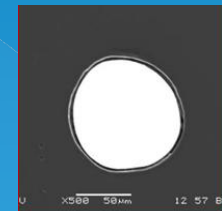
Squared edges



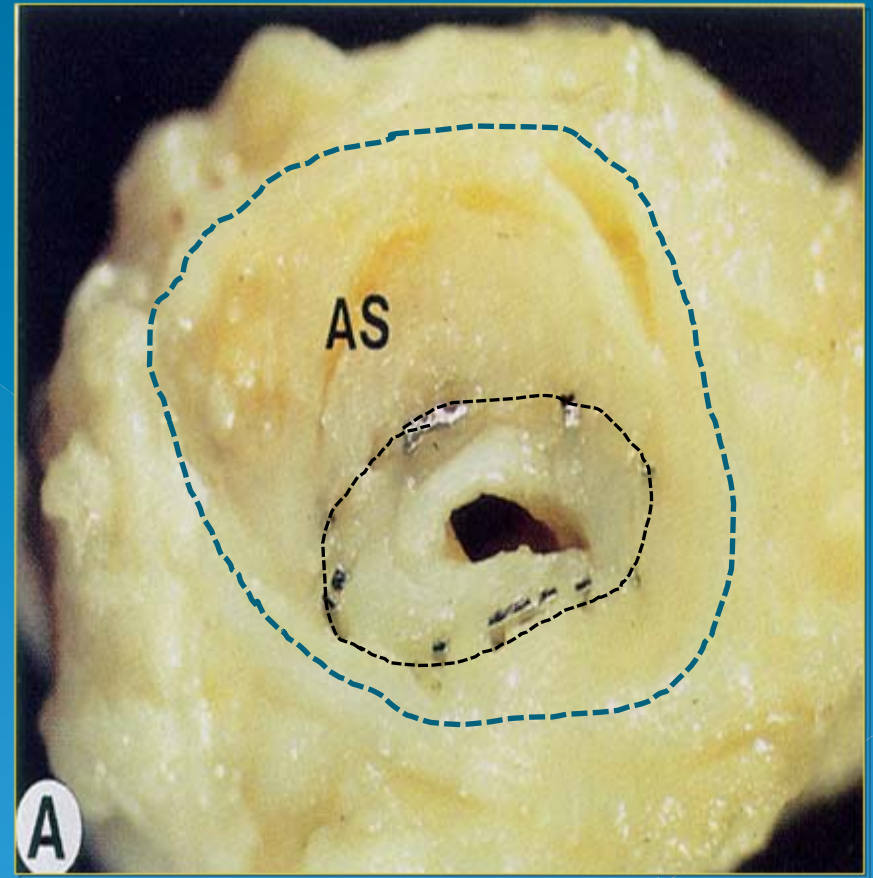
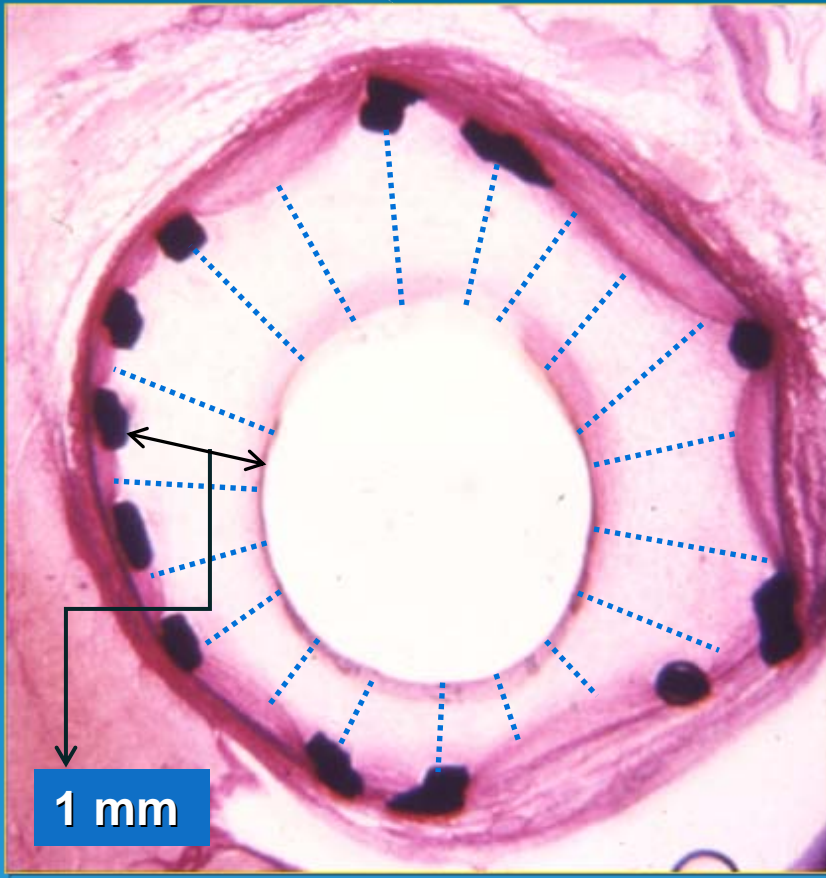
2. **Metallic rings** are formed into sinusoidal elements that are fused together to comprise a modular stent.



Ultrathin, smooth, edgeless struts



The Limitation of Bare Metal Stents



In-stent Restenosis = Intimal Hyperplasia

Drug-Eluting Stents

First Generation

Stent design and delivery system

Drug-
Eluting
Stent

DRUG

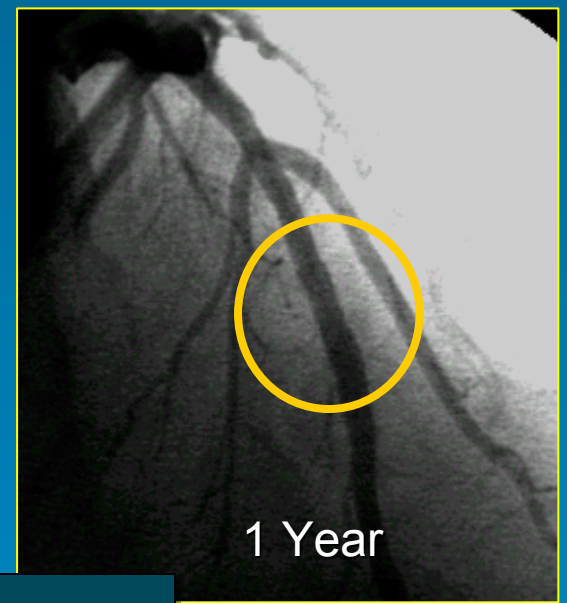
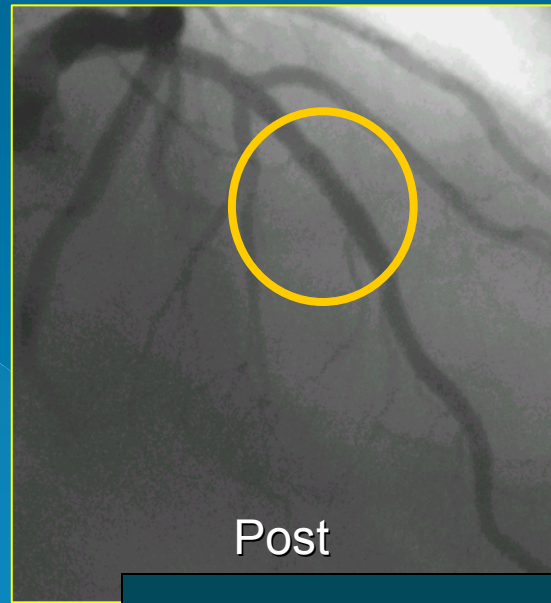
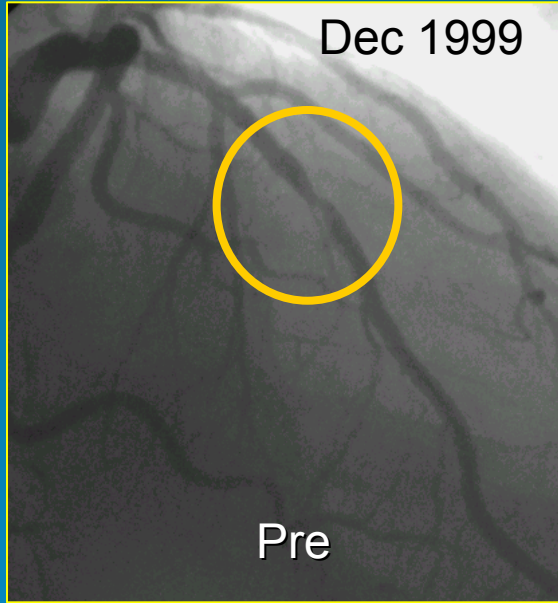
Known FDA-approved
drugs with approximated
release kinetics

“Off the shelf” outdated
stent and delivery system

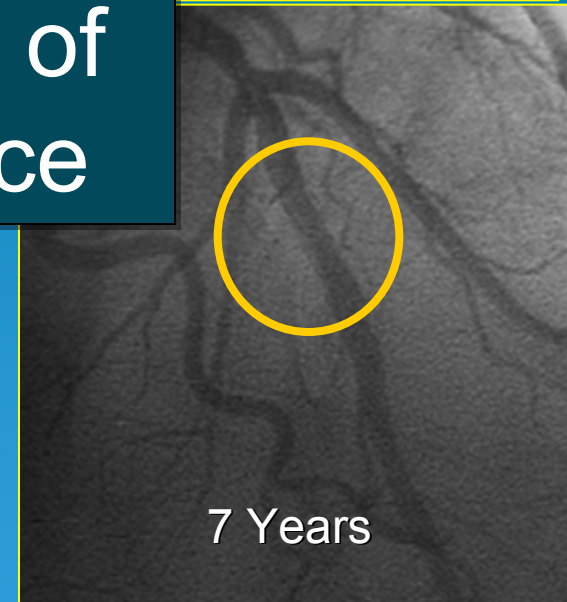
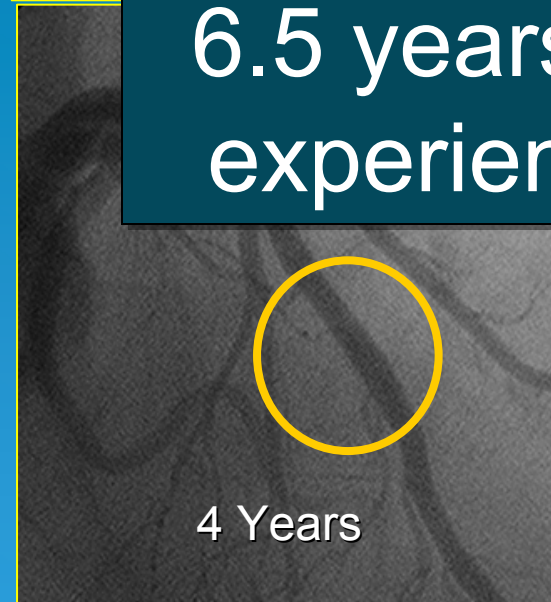
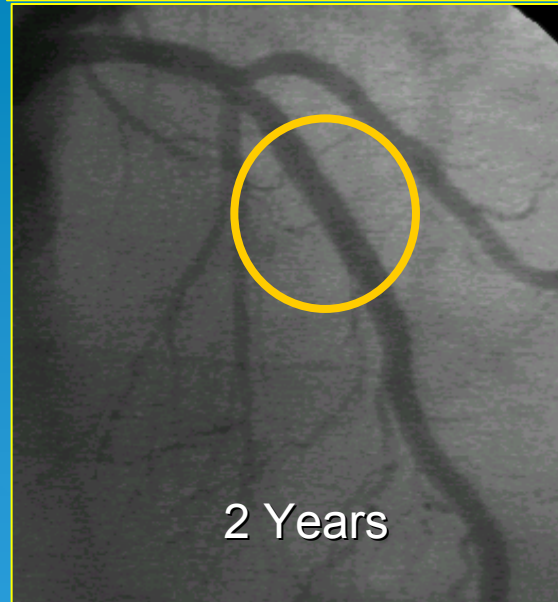
Drug carrier
vehicle

Available, FDA-approved
biostable polymers

CYPHER Stent: First patient 7 Years FU



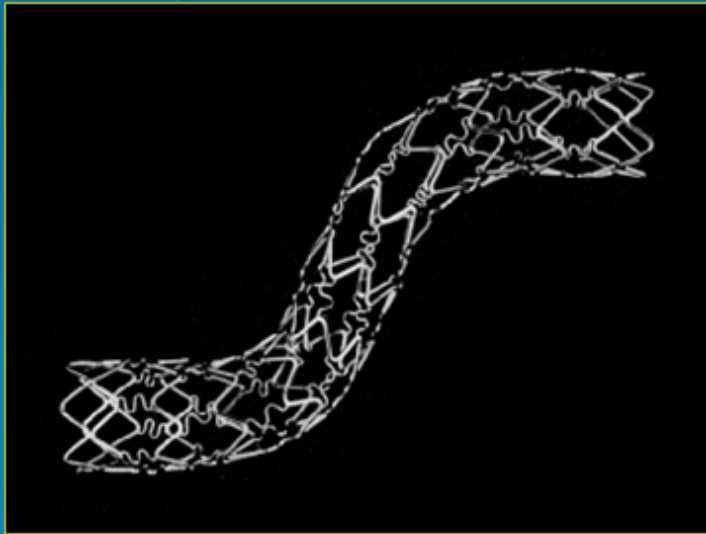
6.5 years of
experience



Success over In-Stent Restenosis!!



The Sirolimus-Eluting Stent (Cypher)

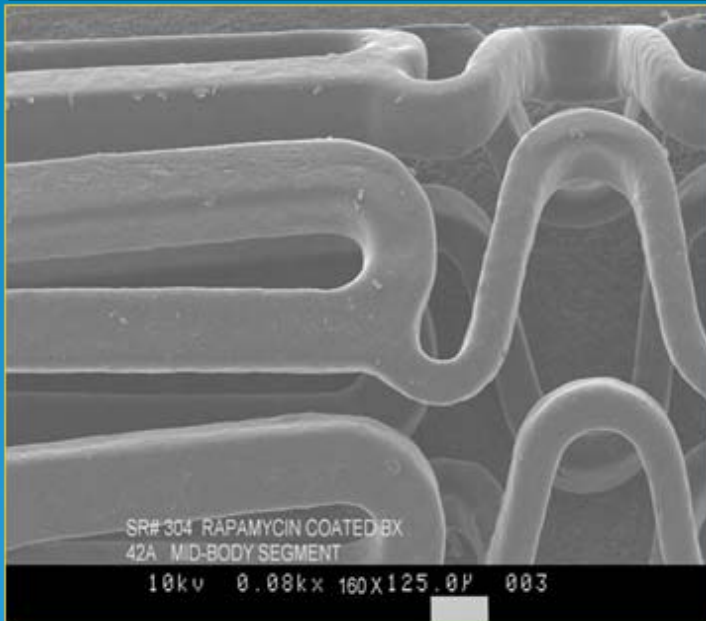


- ***Bx VELOCITY™ Stent***

Stainless steel stent

- Coating:

Blend of 2 polymers (PEVA + PBMA) containing Drug:
Sirolimus (~ 10um thick)



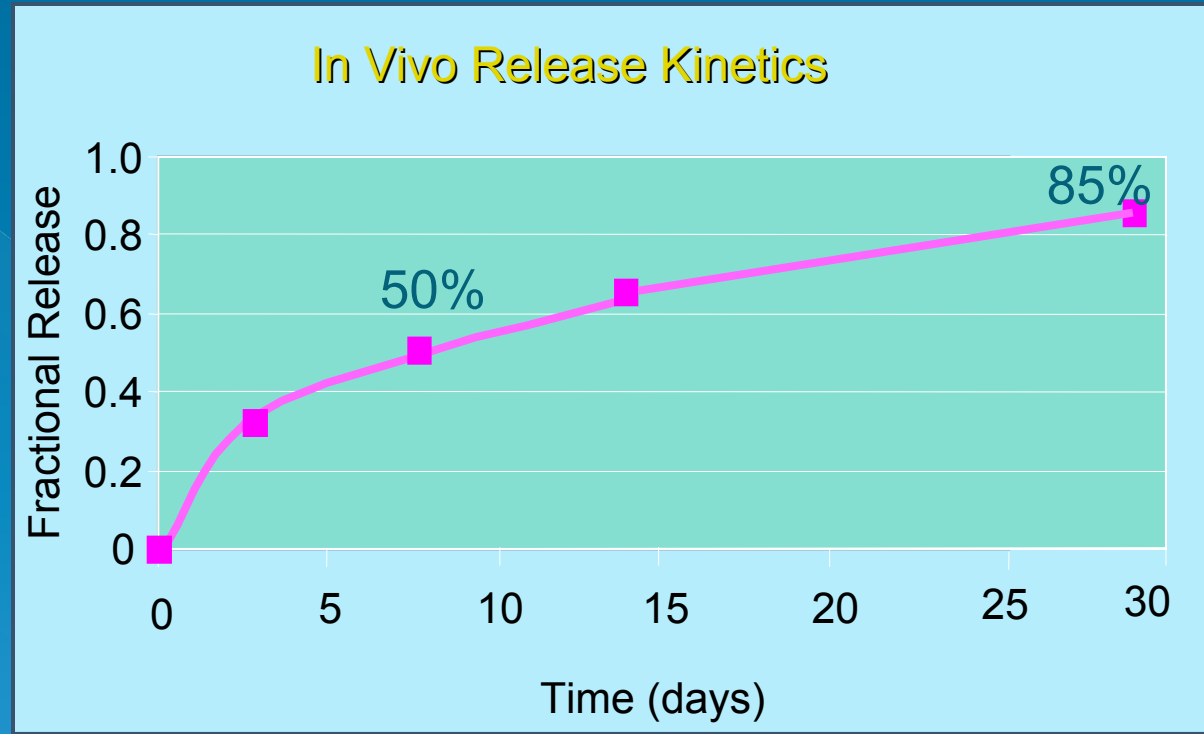
Sirolimus Eluting Cypher Stent

Topcoat



Basecoat = polymer/drug
+

Topcoat = polymer only
(diffusion barrier)

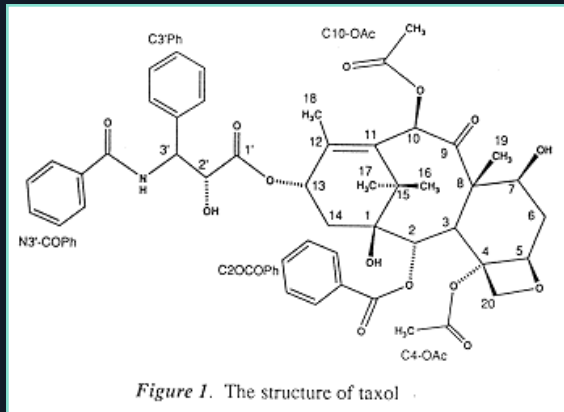


Sirolimus (Rapamycin): Cytostatic Agent

Released in a controlled manner from the polymer matrix (PEVA + PBMA)
ALL of the drug is released within 3 months

One Year later: TAXUS Stent

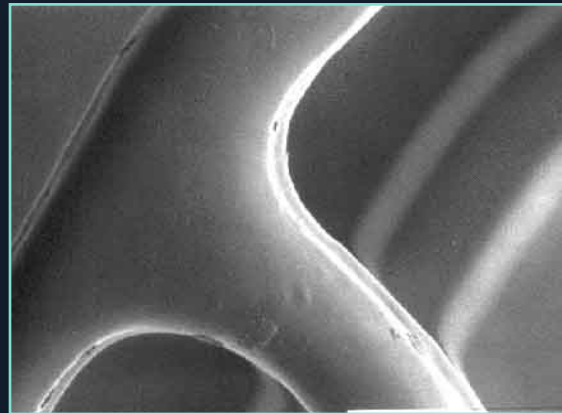
Drug



Paclitaxel

- Binds tubulin
- Stabilizes microtubular deconstruction
- Multi-cellular
- Multi-functional
- Cytostatic at low dose

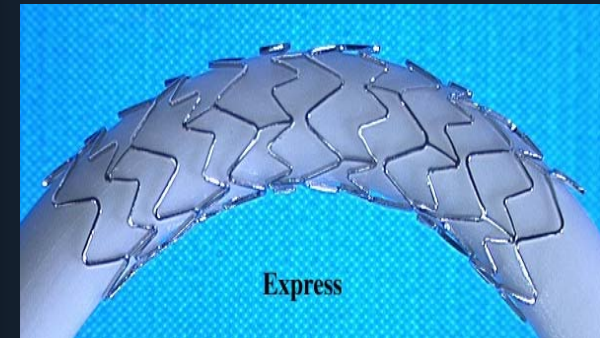
Polymer



Translute™

- Polyolefin derivative
- Uniform
- Biocompatible
- Elastomeric
- Provides controlled release

Stent



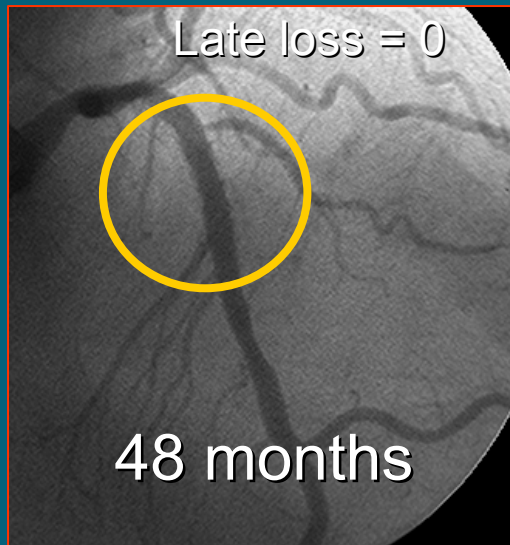
Express²

- Tandem architecture
- Maverick balloon system
- Flexible
- Deliverable

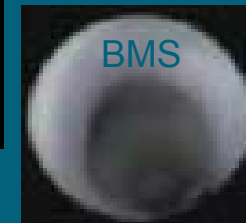
Look Carefully !!



1st Generation DES.... the good, the bad, and the ugly!

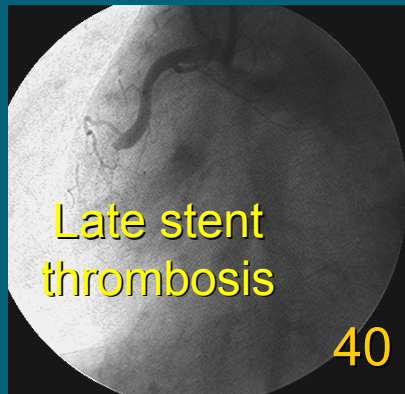


Angioscopy

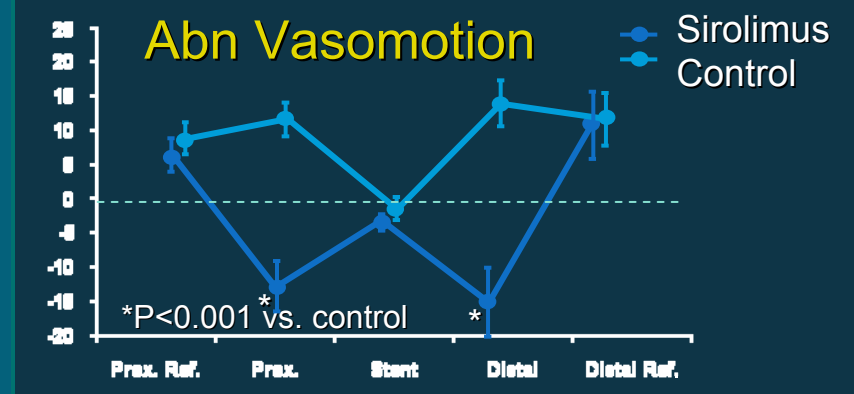
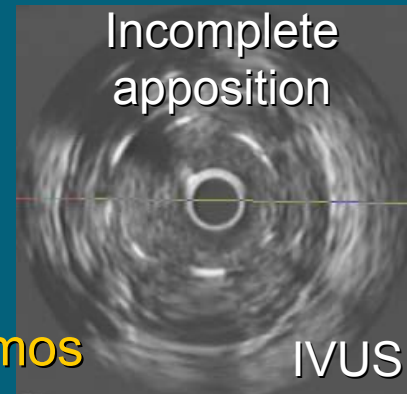


Inflammation

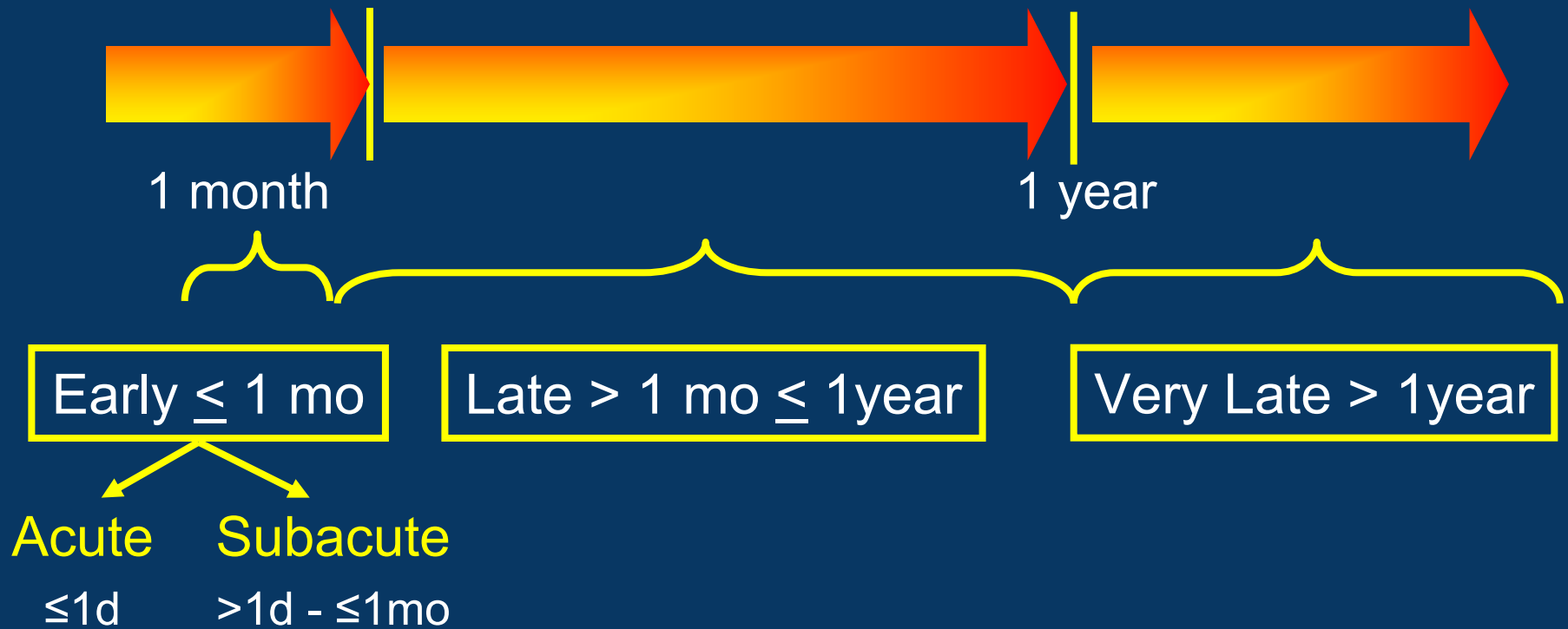
Delayed Healing!



40 mos

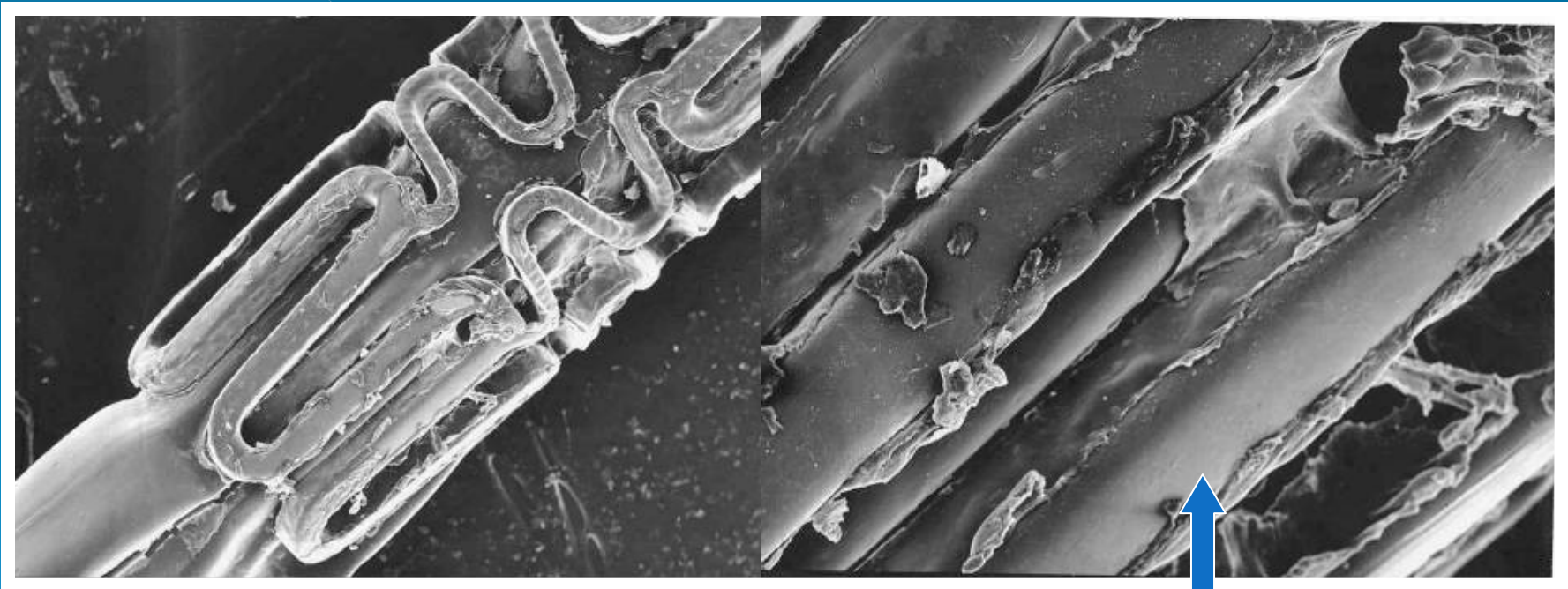


Stent Thrombosis

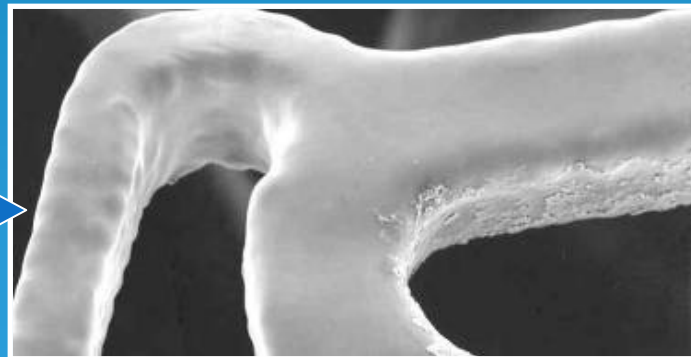


And still some restenosis.....

Polymer coating damage



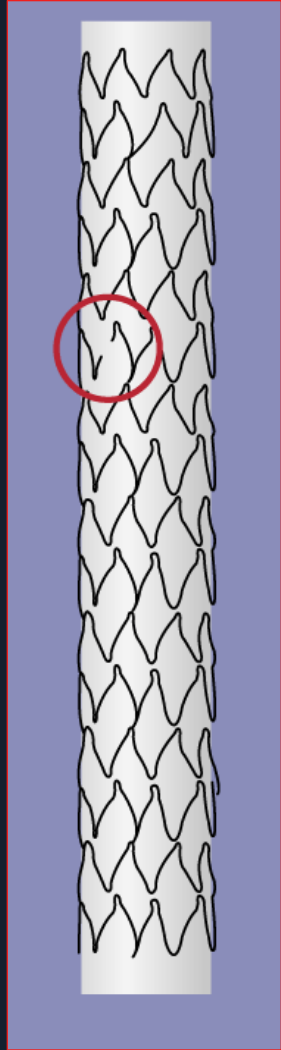
*Undamaged
polymer*



*Failed to cross
calcified lesion*

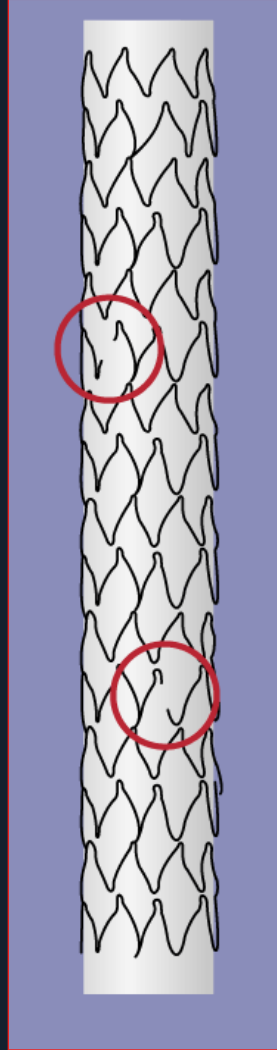


Type I



Single strut fracture

Type II



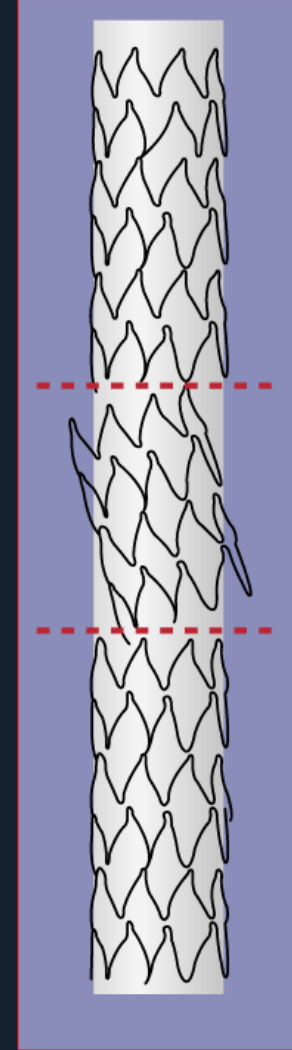
Multiple single stent fractures; different sites

Type III



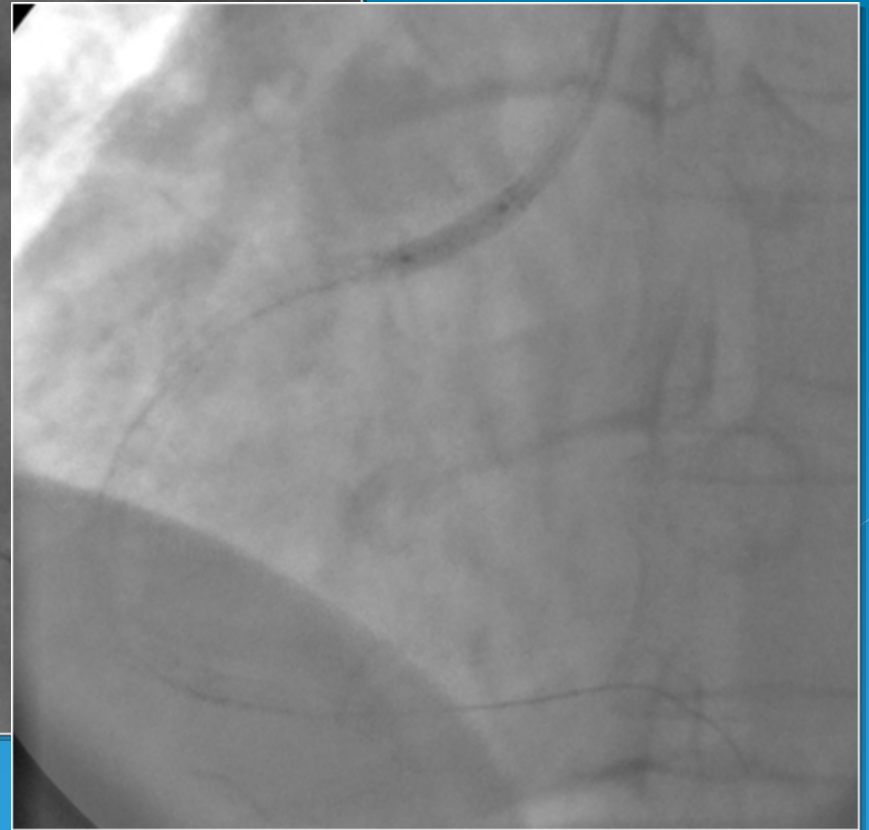
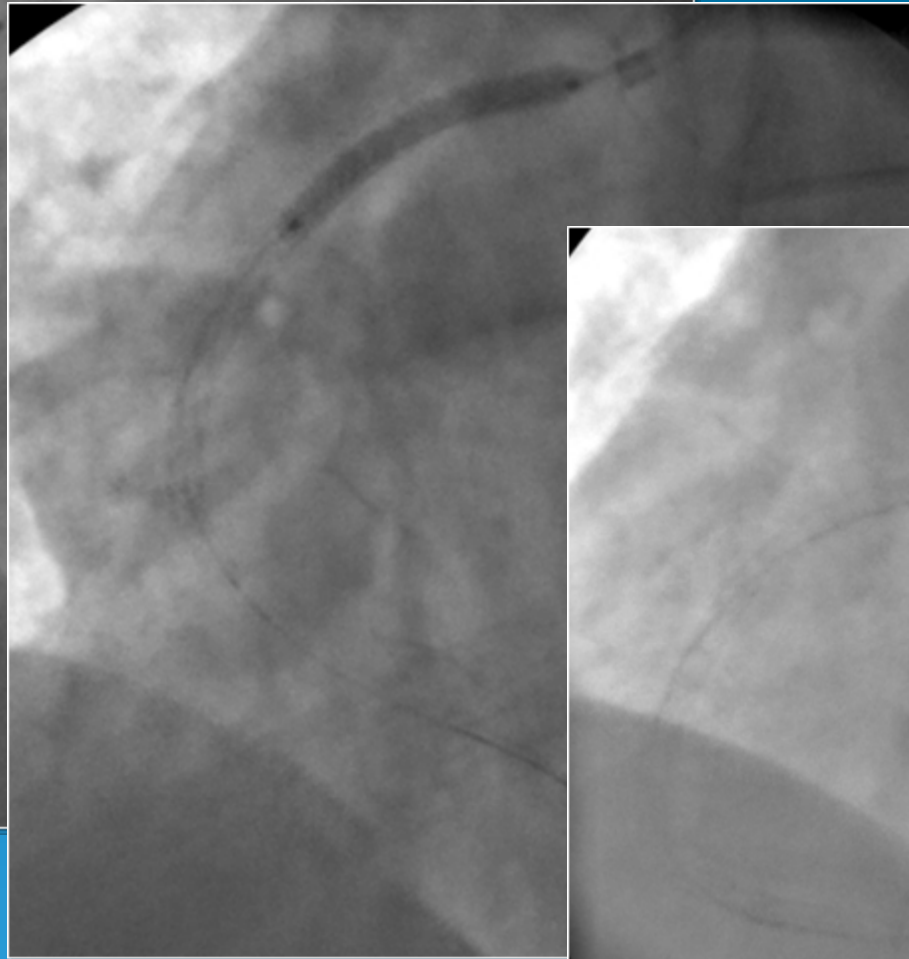
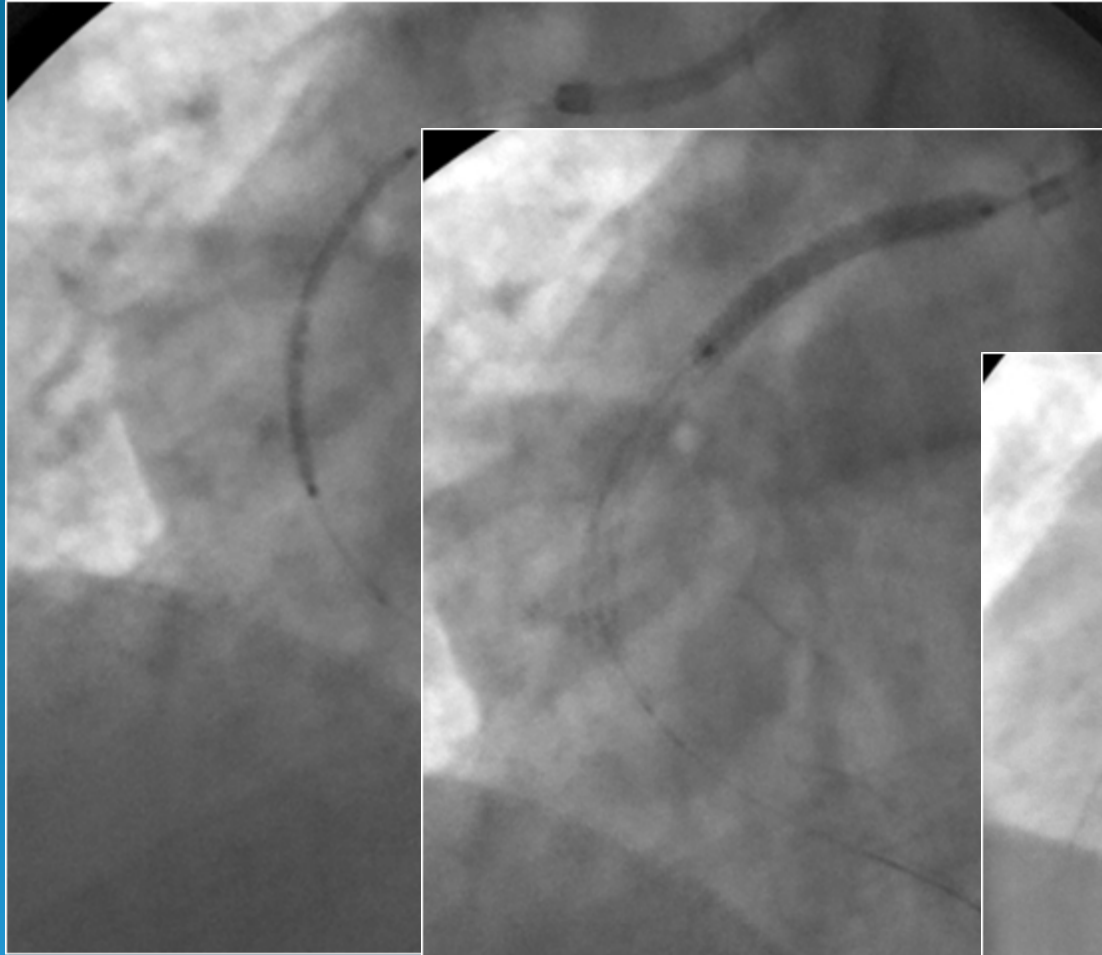
Multiple stent fractures; complete transverse linear fracture

Type IV

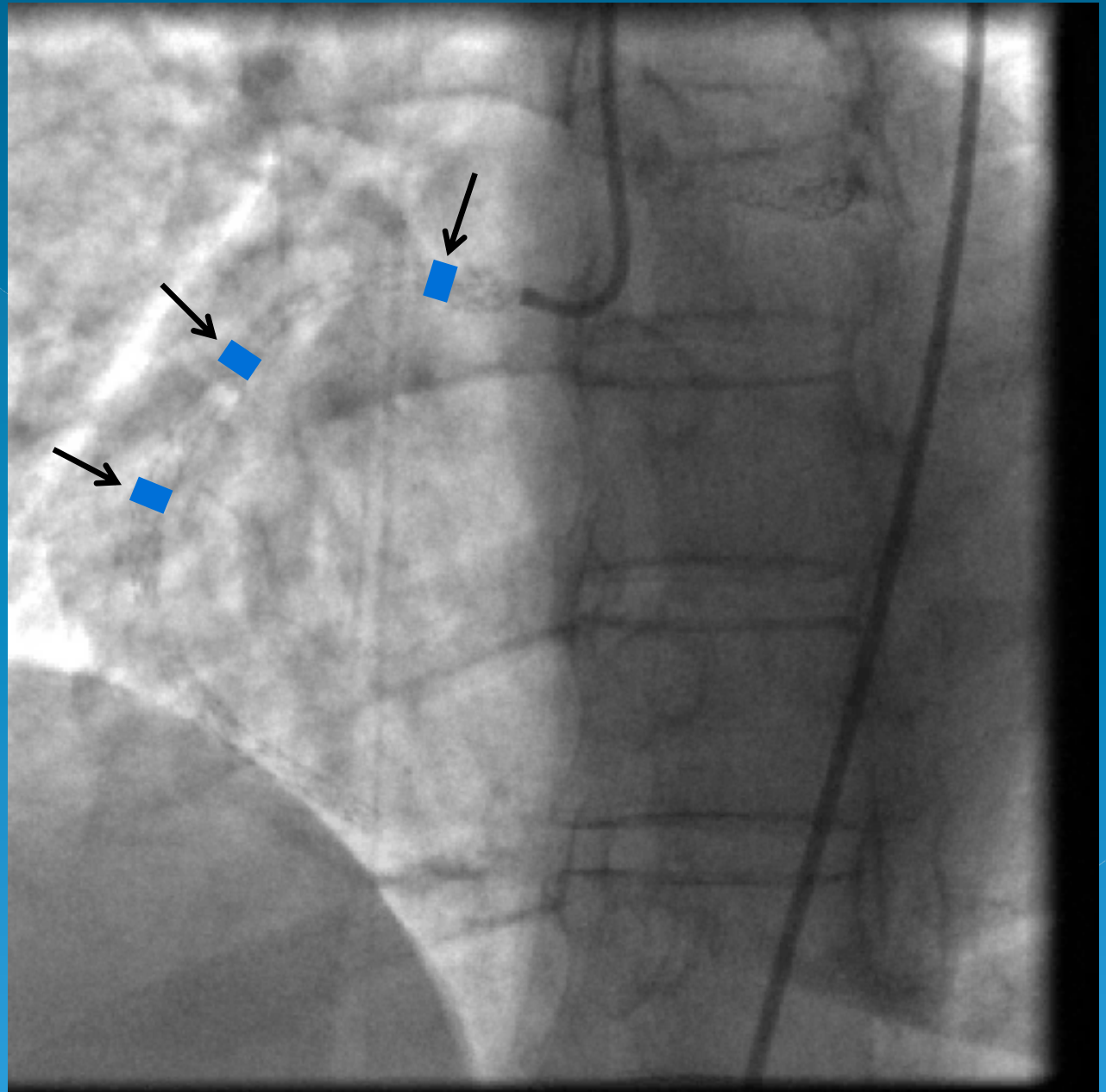


Complete transverse linear Type III fracture with stent displacement

RCA STENT PLACEMENT FOR DIFFUSE DISEASE



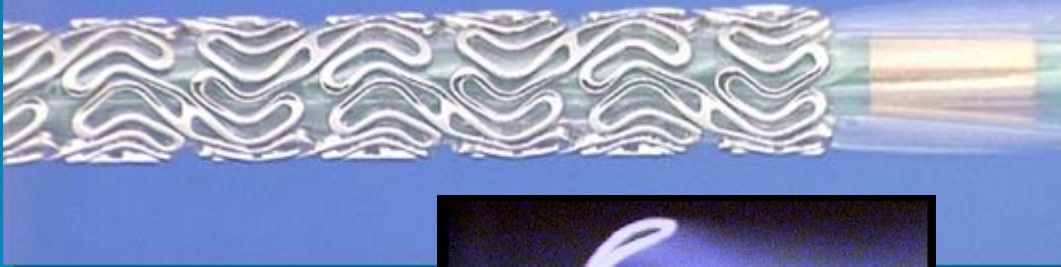
More than 2
yrs later, stops
DAPT. One
week later
comes in with a
inferior STEMI:
Multiple
Cypher stent
Fractures



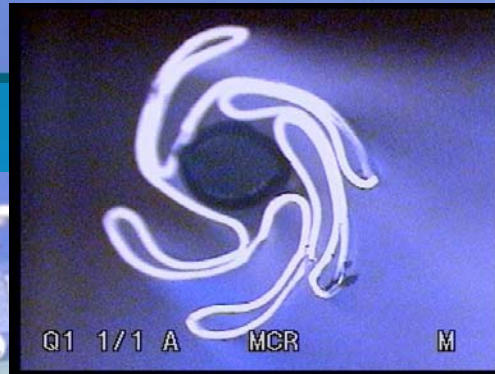
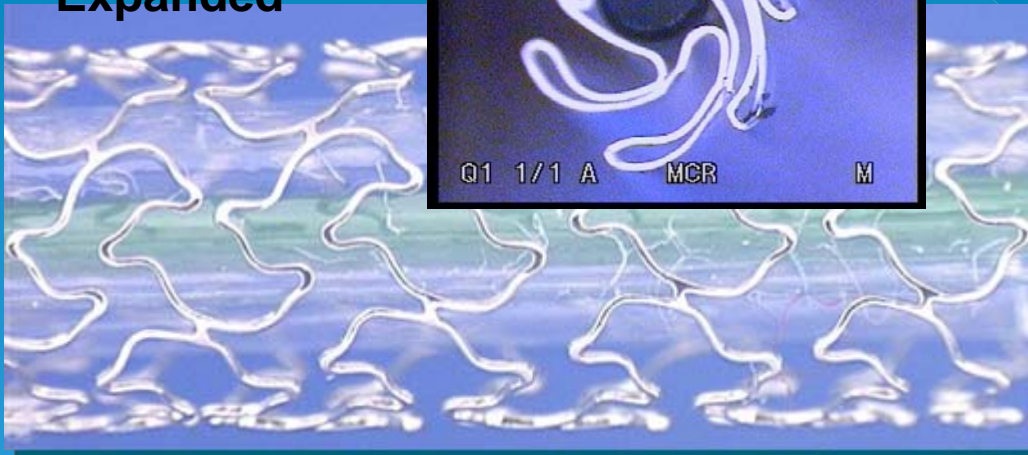
Second Generation DES: Better designed to be drug eluting stents

Second Generation TAXUS Stent: TAXUS Liberté™

Crimped



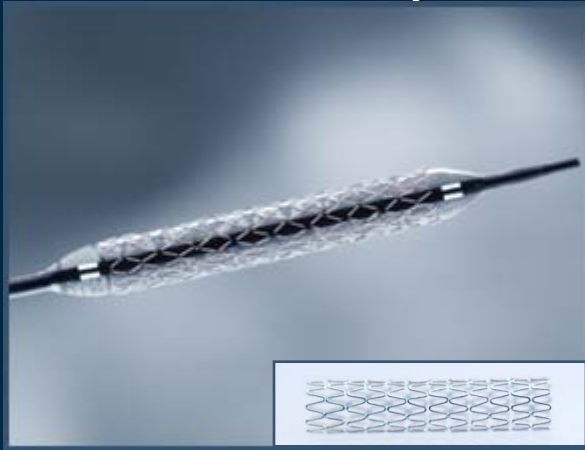
Expanded



- *Polymer and drug are unchanged*
- *Maverick² balloon*
- *5-wing fold for improved re-wrap and less resistance to withdrawal*
- *Stainless steel 27%↓ in strut thickness - from 0.0052" (Express²) to 0.0038"*

Endeavor DES System

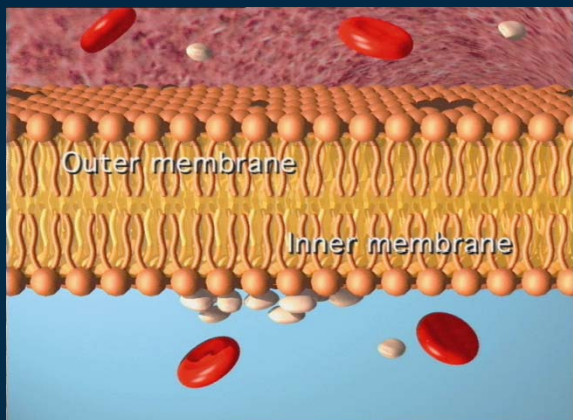
Driver Cobalt Alloy Stent



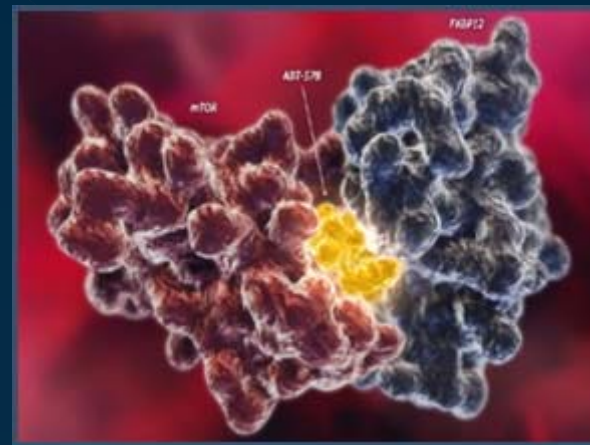
Stent Delivery



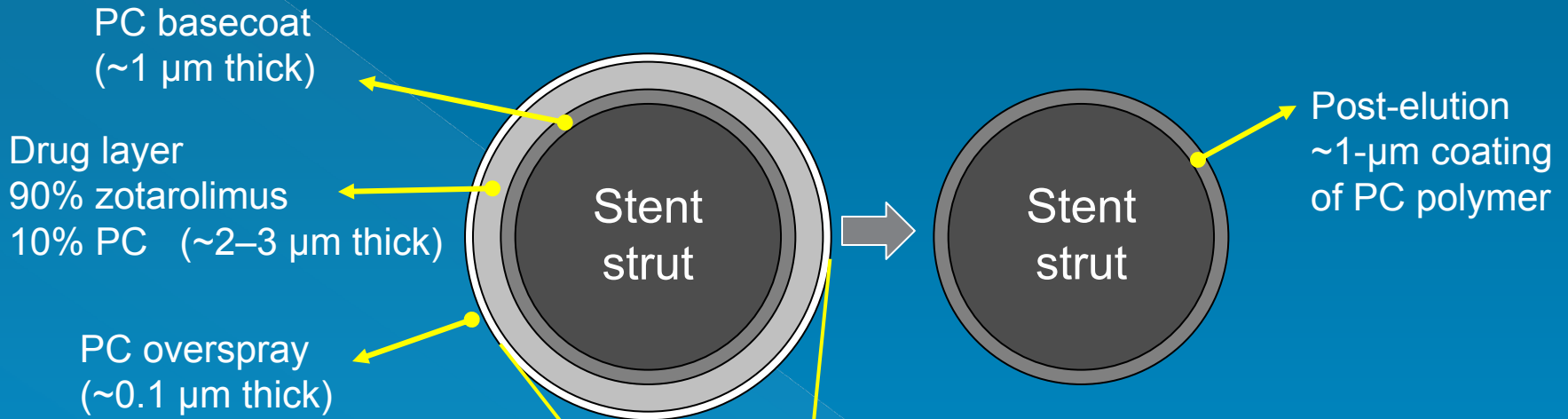
PC Technology



Drug: Zotarolimus



Endeavor Polymer + Drug Matrix

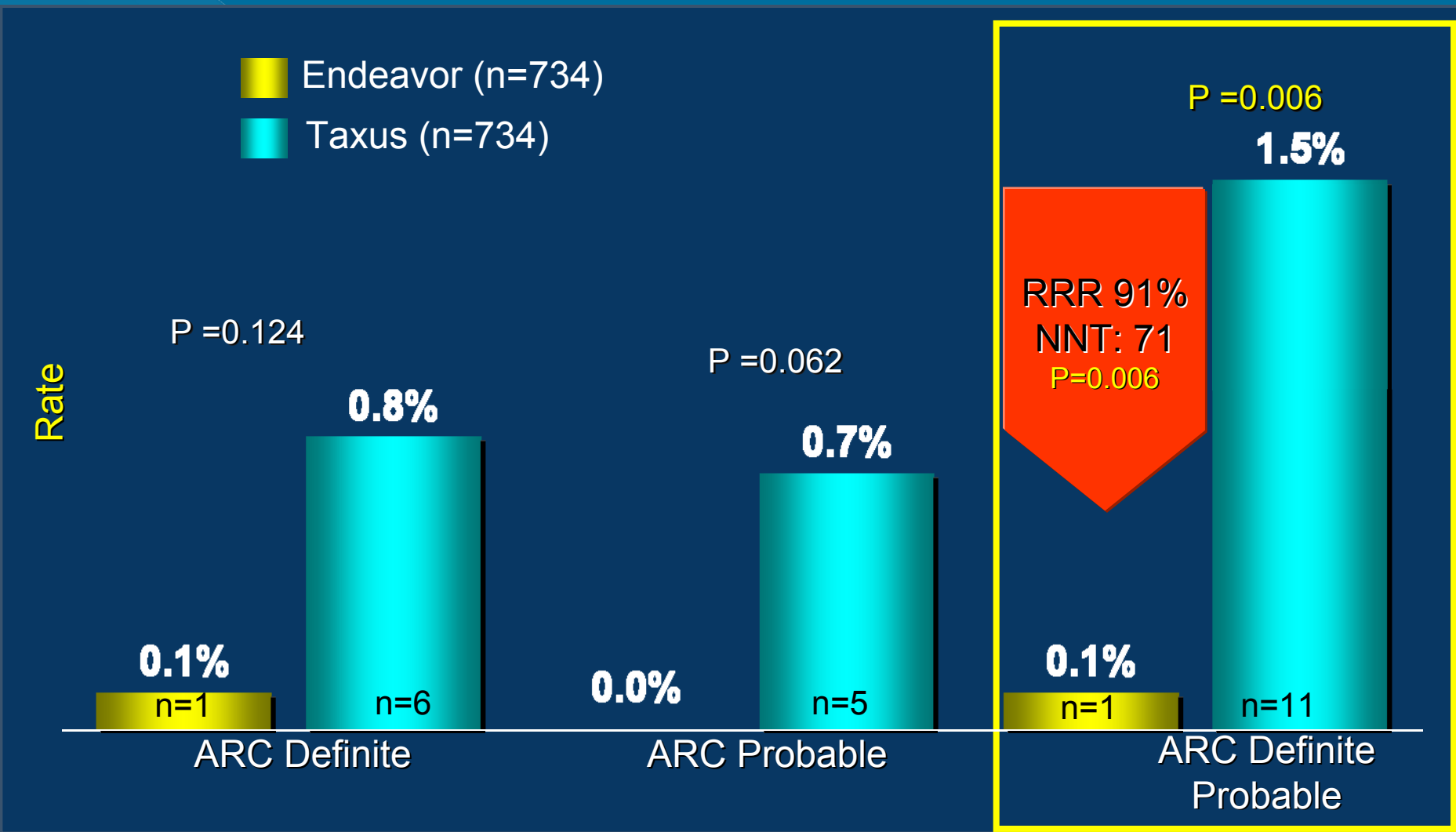


3.0-mm stents
500x magnification

	Endeavor	Taxus [®]	Cypher [®]
Drug/polymer	4 μm	16 μm	13 μm
Strut thickness	91 μm	132 μm	140 μm
Total thickness	95 μm	148 μm	153 μm

Very Late Stent Thrombosis (12-36 mos)

ENDEAVOR IV – 3yr FU

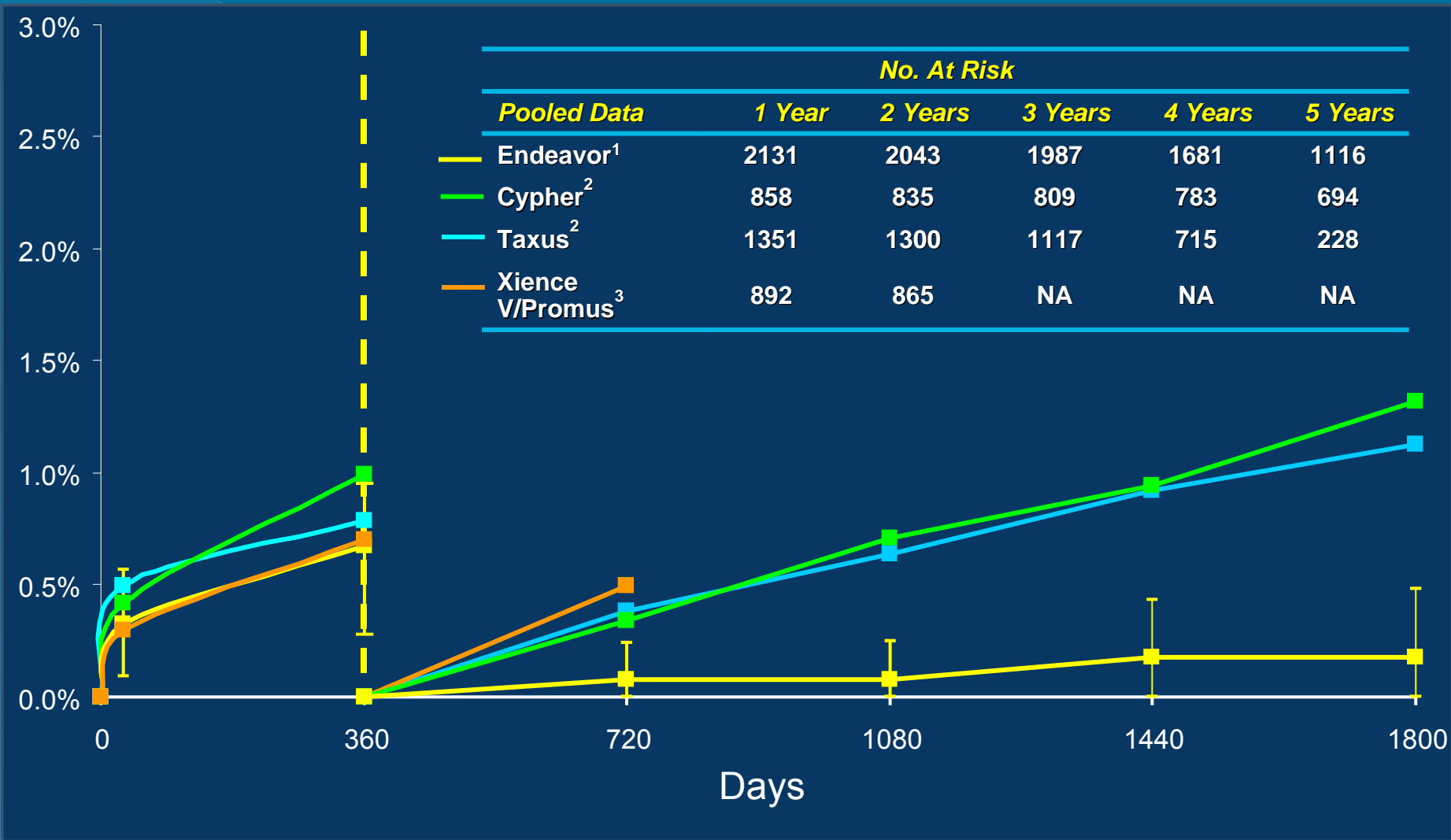


* ARC definition

TCT Sep 2009

DES Pooled Programs

Definite/Prob ST* Landmark at 1 year to 5 Years



*ARC Def

1. Mauri et al. PCR 2009.

2. 5 year Outcomes in the Sirius Trial, Weisz et al. JACC Vol. 53, No. 17, 2009

3. Mauri L et al. N Engl J Med. 2007;356:1020-1029.

4. Stone, G et al., New SPIRIT Clinical Data, ACC 09.

OPTIMIZE (Brazil)

RCT 3 months DAPT vs 12 months

All comers (excluding STEMI)
Reference Vessel Diameter 2.25 mm-4.0 mm

Endeavor Stent
3 months DAPT
n = 1,600

N = 3,200 patients
in
Brazil

Endeavor Stent
12 months DAPT
n = 1,600

Clinical/MACE

30d

6mo

12mo

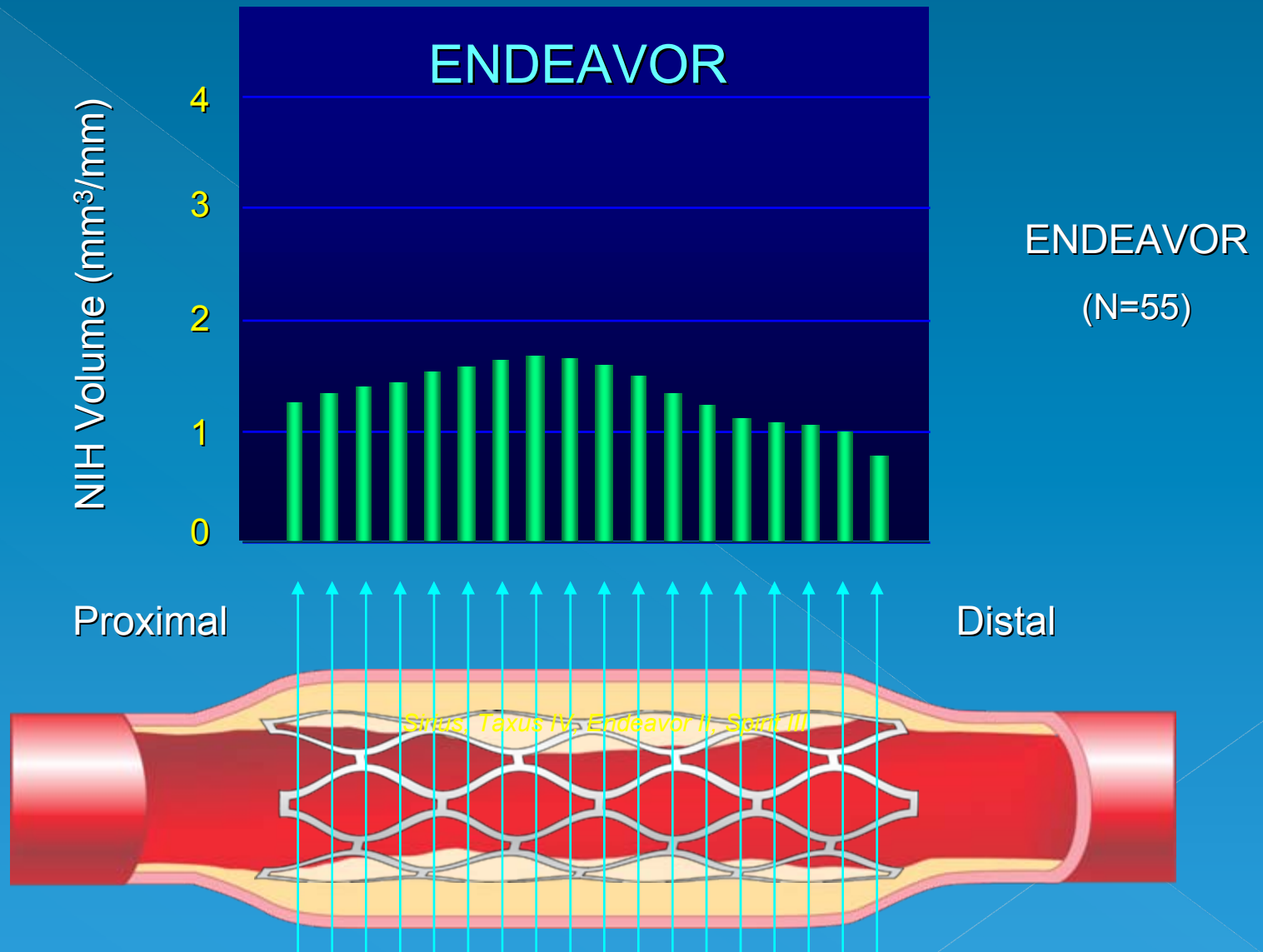
15 mo

Primary Endpoint: TLF at 12 months

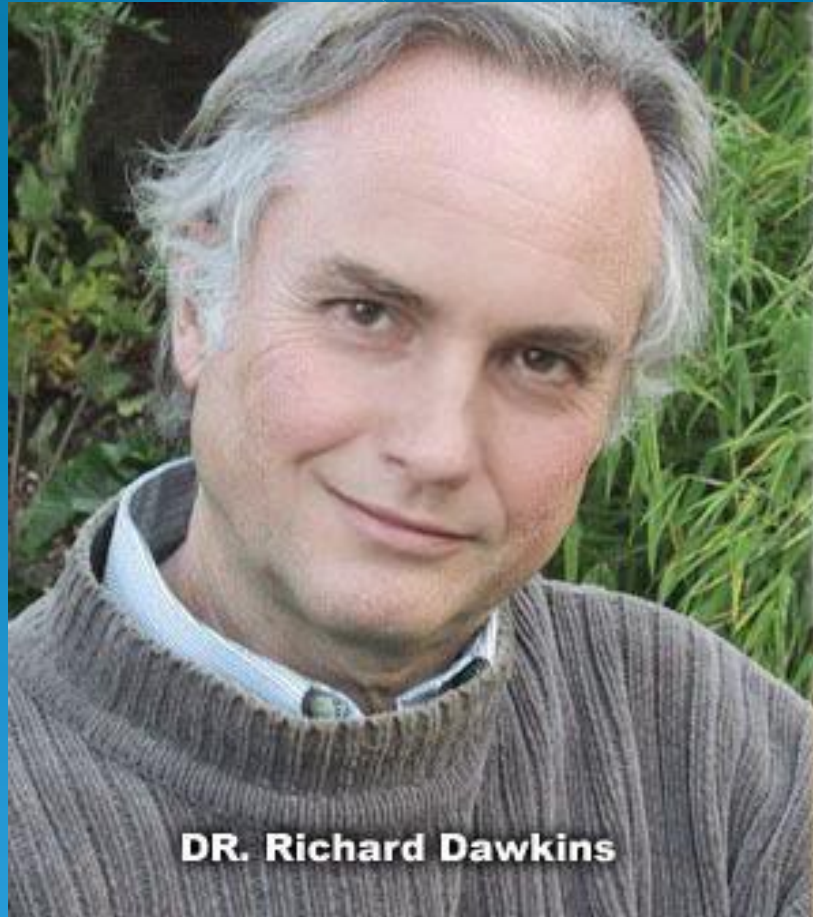
Secondary Endpoints: MI, Cardiac Death, ARC def/prob ST at 30 days,
6 months and 15 months

Drug Therapy: ASA and Clopidogrel 3 or 12 months

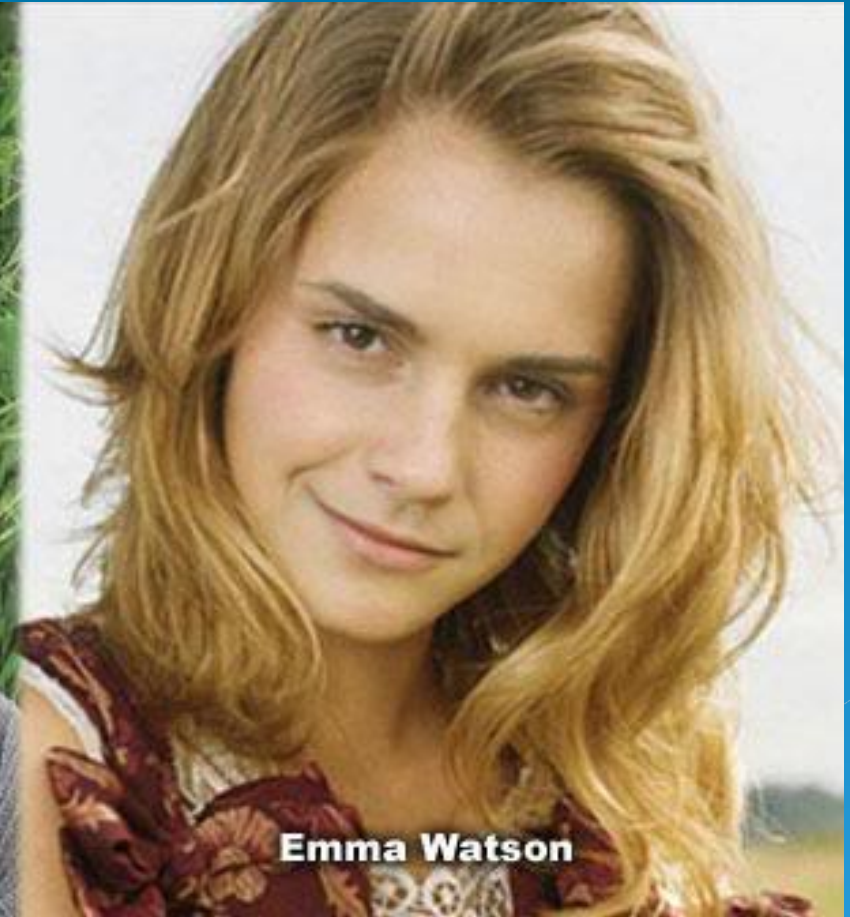
ENDEAVOR – IVUS



DES: They look similar but they are not the same



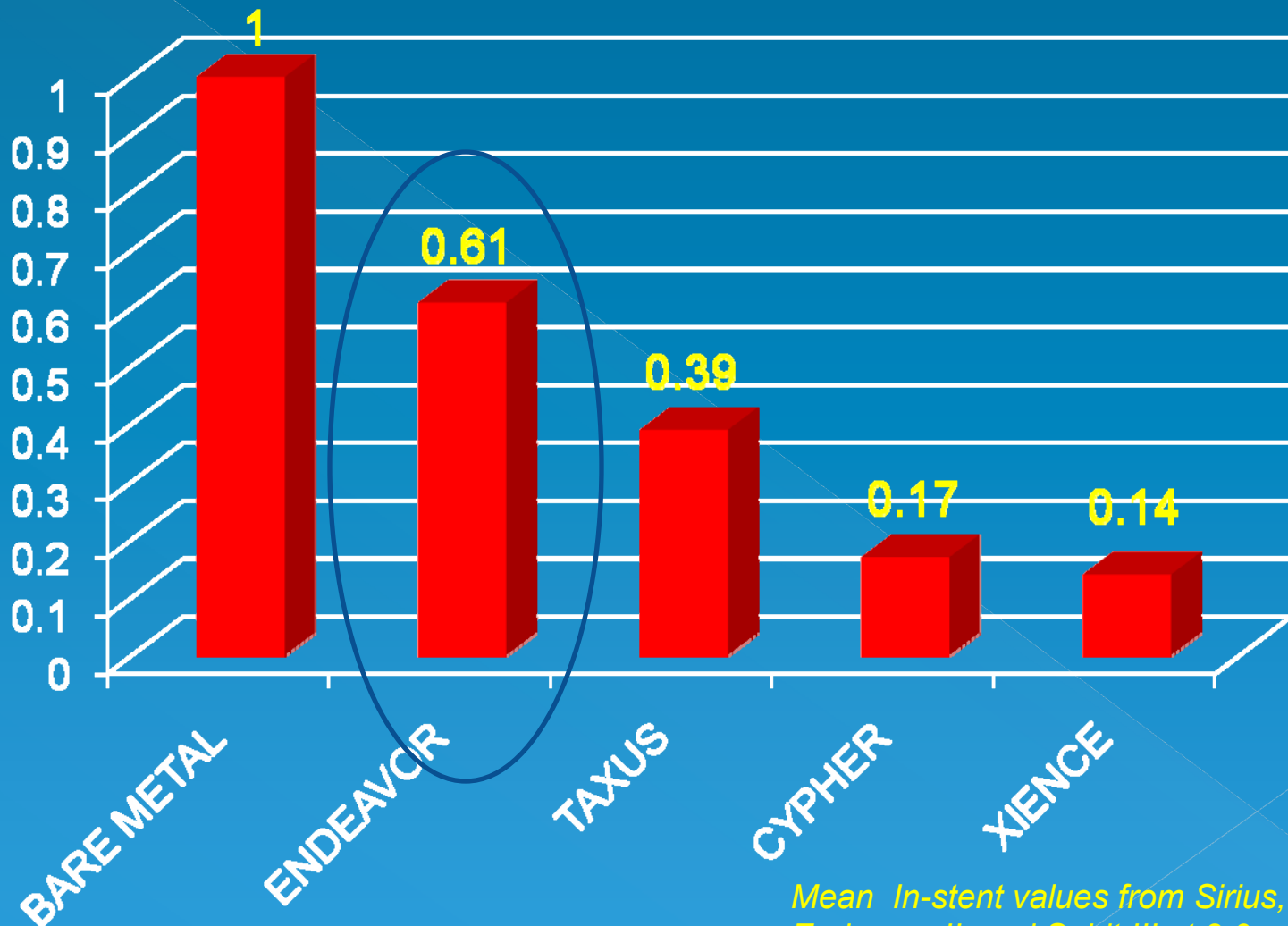
DR. Richard Dawkins



Emma Watson

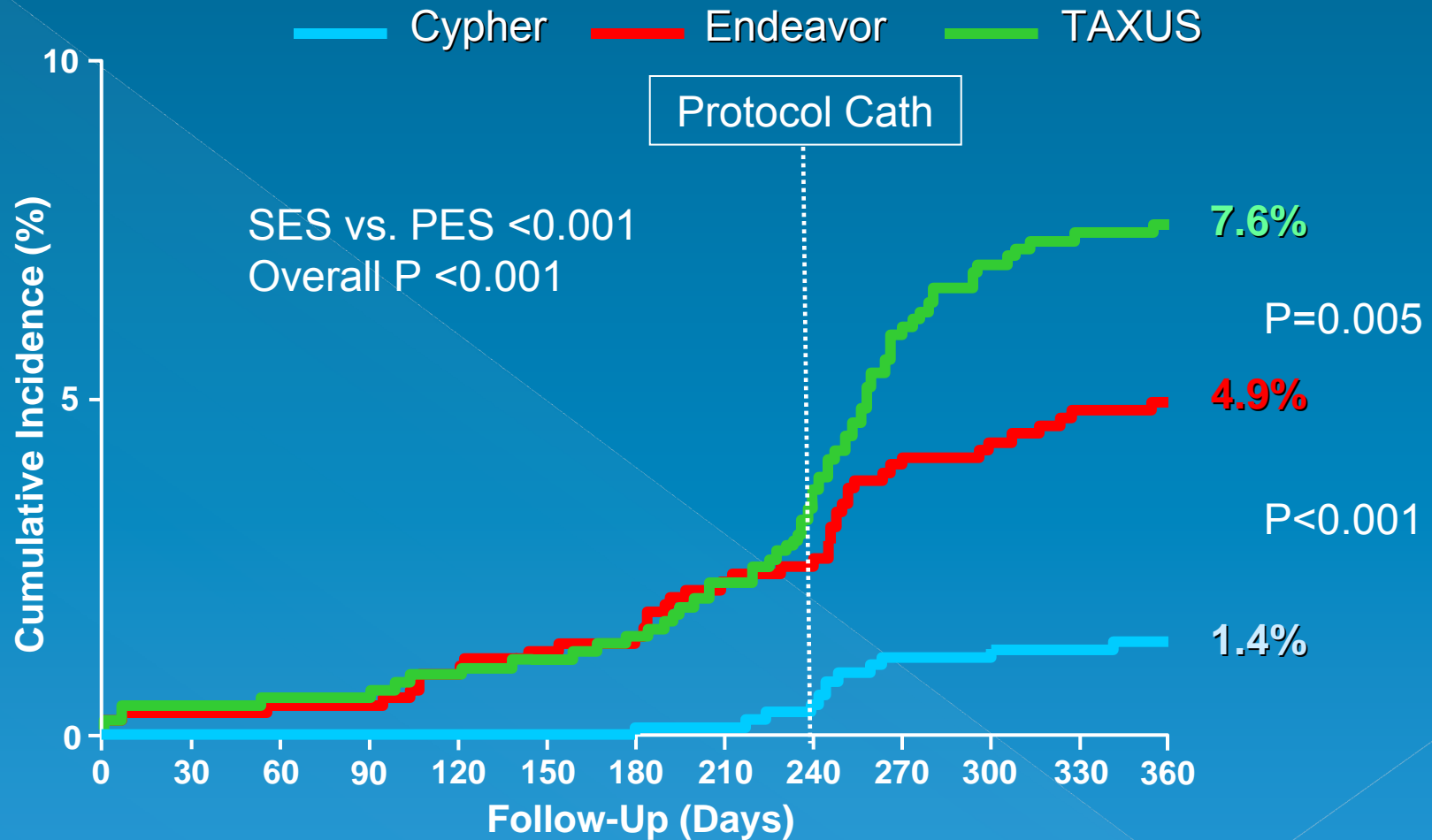
Late Loss* (mm)

An (imperfect) Index of Anti-restenotic Efficacy



Mean In-stent values from Sirius, Taxus IV Endeavor II, and Spirit III at 8-9 months

Ischemic driven TLR



Zest Trial, 2009

Solution: Resolute DES System

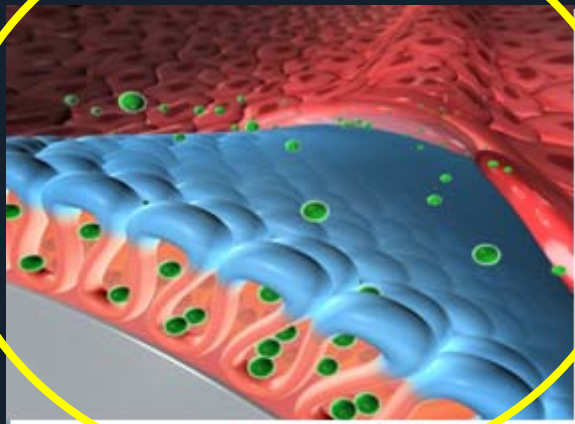
Driver Cobalt Alloy Stent



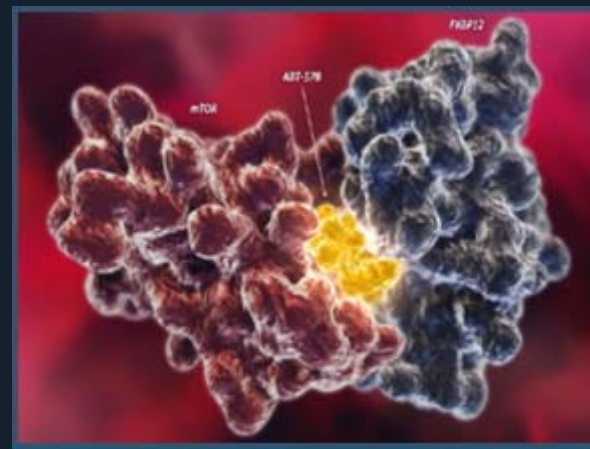
Stent Delivery System



BioLinx Polymer

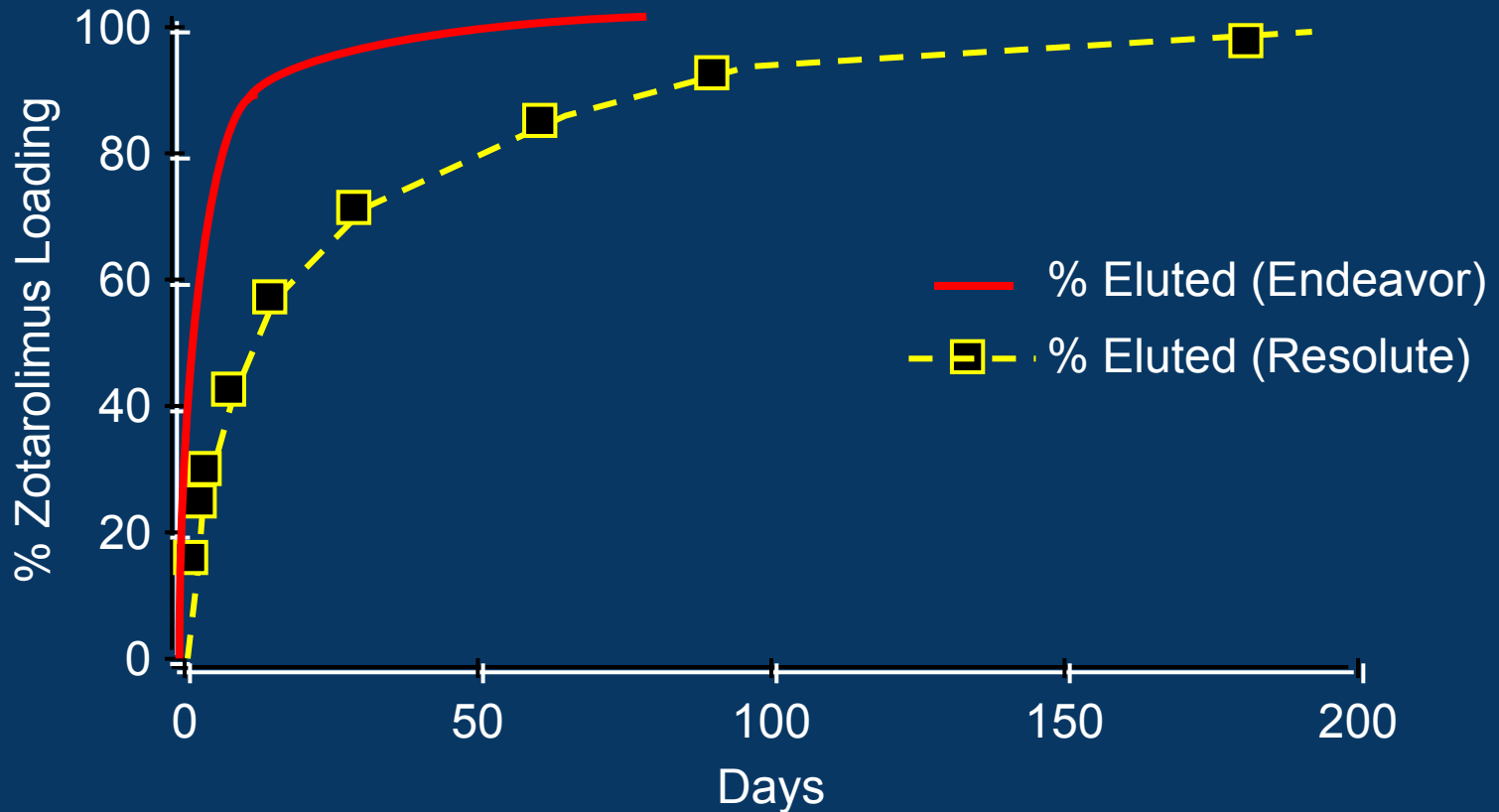


Drug: Zotarolimus



Resolute Elution Kinetics

BioLinx Polymer in vivo Elution



Greater than 85% of the drug is eluted at 60 days
Complete drug content exhausted by 180 days

Endeavor RESOLUTE

9 month Angiographic Results

n=96	In-stent	In-segment
Pre-procedure RVD (mm)		2.79 ± 0.40
Lesion Length (mm)		15.87 ± 6.51
MLD (mm) pre		0.82 ± 0.35
post	2.74 ± 0.41	2.33 ± 0.44
Acute Gain	1.91 ± 0.47	1.51 ± 0.50
Late loss (mm) ENDEAVOR	0.67 ± 0.49	0.42 ± 0.50
Late Loss (mm)	0.22 ± 0.27	0.12 ± 0.27
Late Loss Index	0.12 ± 0.16	0.08 ± 0.21
9 mo f/u % DS	10.13 ± 12.63	21.08 ± 10.62
ABR n (%)	1 (1%)	2 (2.1%)

COMING SOON.....

Continuous Sinusoid Technology and Stent strut construction

Continuous Sinusoid Technology



Program Targets:

- Enhance deliverability and conformability without compromising strength & opacity
- Develop a platform for DES that enables optimized drug transmission

0.0038"



0.0034"



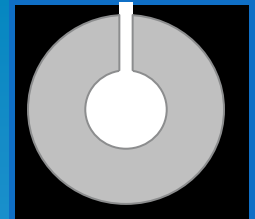
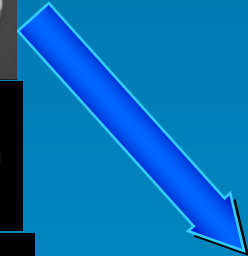
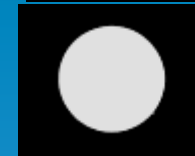
0.0030"



0.0025"



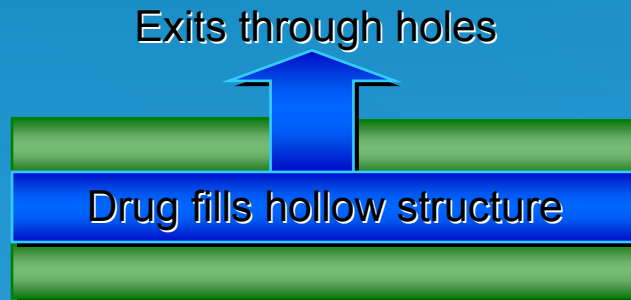
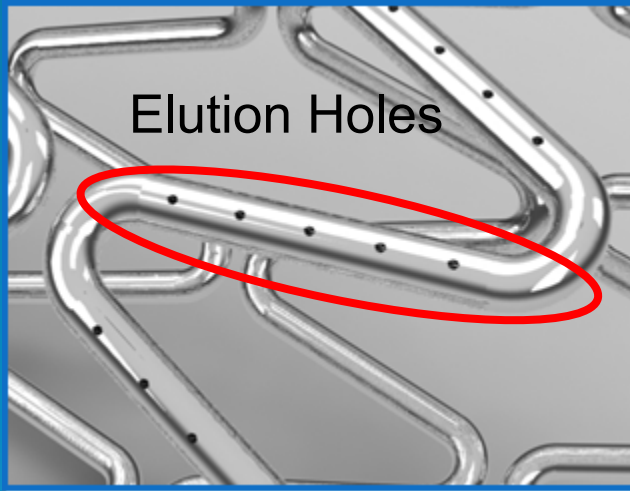
0.0020"



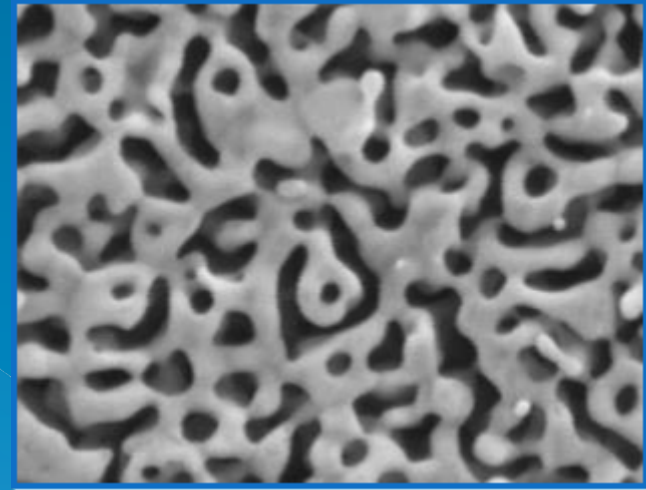
Drug-Filled Stent

Non-Polymeric DES Approaches

Drug-Filled Stent



Nanoporous Surface Modification



Development Targets:

- Inhibit restenosis and cell proliferation without the use of a polymer
- Provide for rapid, healthy endothelialization

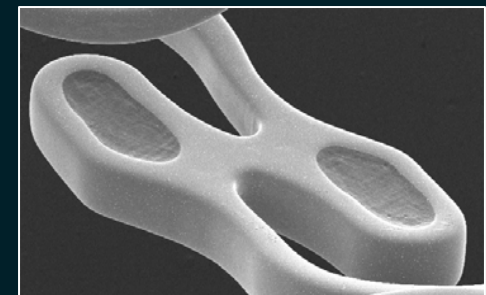
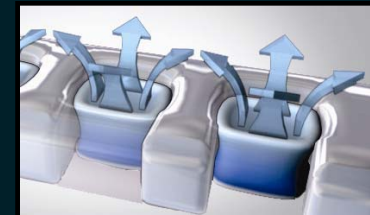
From Cypher to New Cordis RES Technology

CoStar[®] Sirolimus-Eluting Coronary Stent System

A Stent Specifically Designed for Controlled Drug Delivery from a Bioresorbable PLGA Polymer

Costar Stent led
Cordis to design
the Nevo Stent

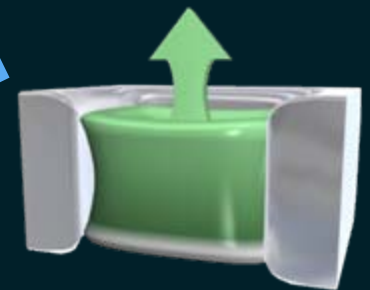
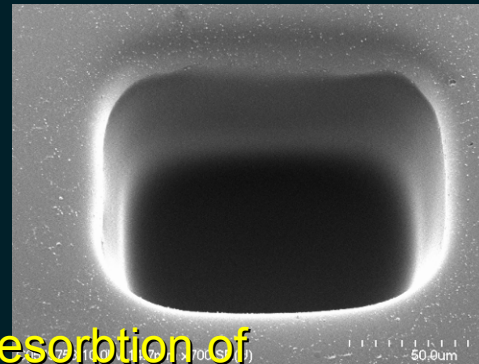
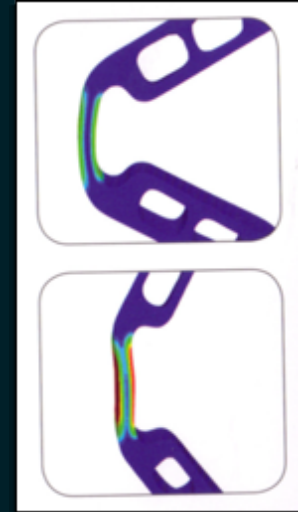
*Reservoir inlays
with PLGA
bioresorbable polymers;
reduced tissue-polymer contact area*



NEVO STENT: Low profile CoCr



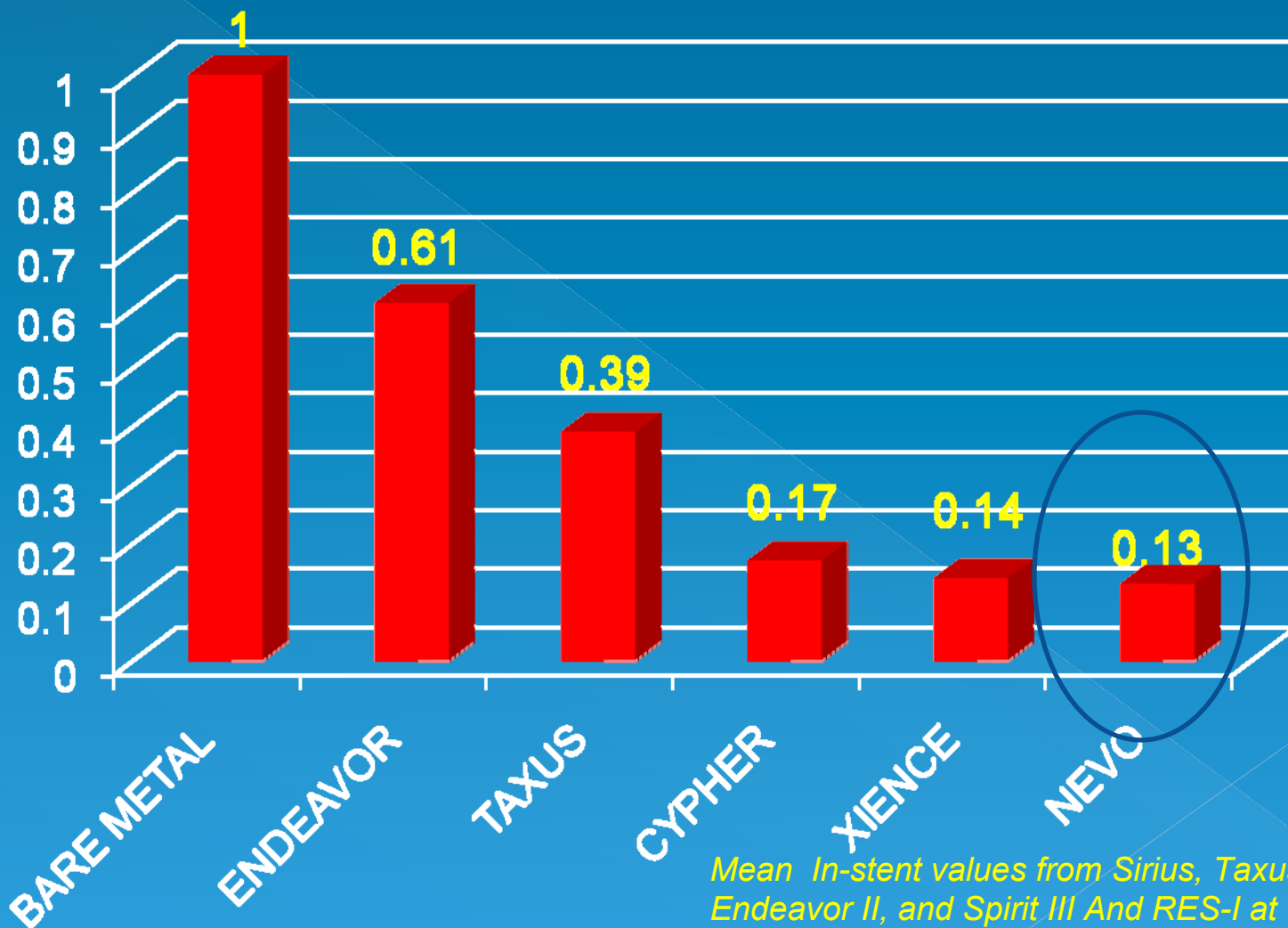
Flexible Design with Non-Deforming Reservoirs



Complete elution of the drug and resorption of the polymer from the reservoirs over time leave behind a bare metal stent

Late Loss* (mm)

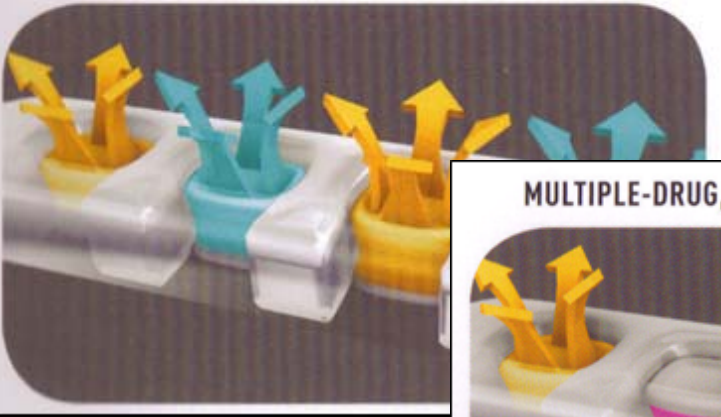
An (imperfect) Index of Anti-restenotic Efficacy



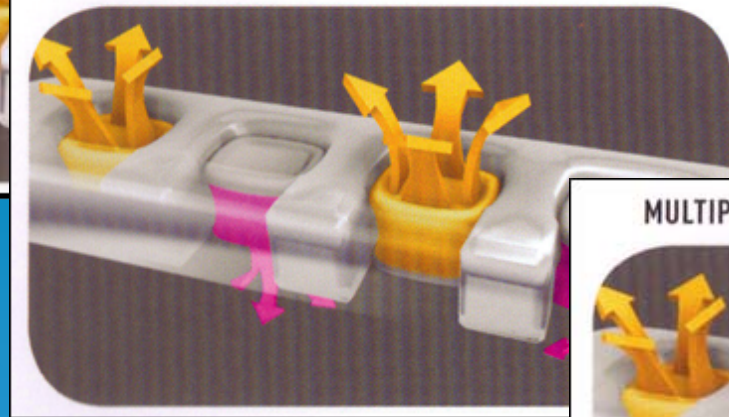
Mean In-stent values from Sirius, Taxus IV, Endeavor II, and Spirit III And RES-I at 6-9 months

Nevo Stent: Future possibilities

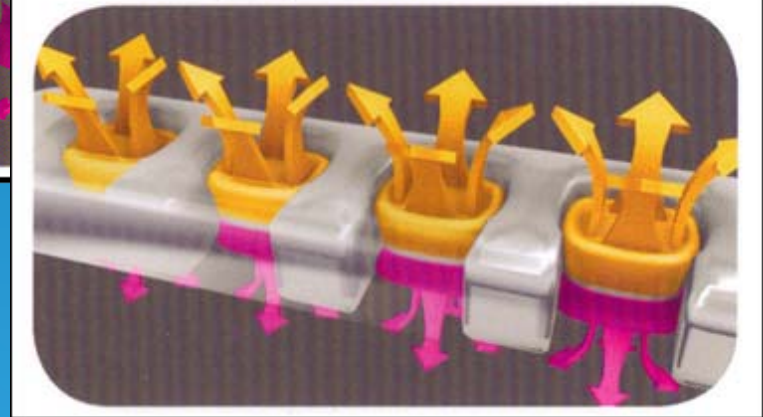
MULTIPLE-DRUG RELEASE



MULTIPLE-DRUG, BIDIRECTIONAL RELEASE



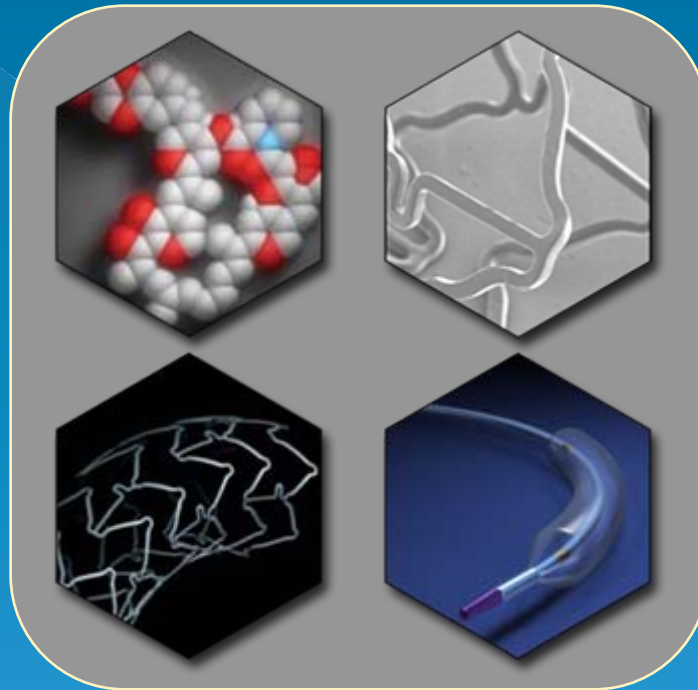
MULTIPLE-DRUG, BIDIRECTIONAL RELEASE



XIENCE V / PROMUS Everolimus-eluting Stent

Everolimus

ML VISION® Stent
Platform

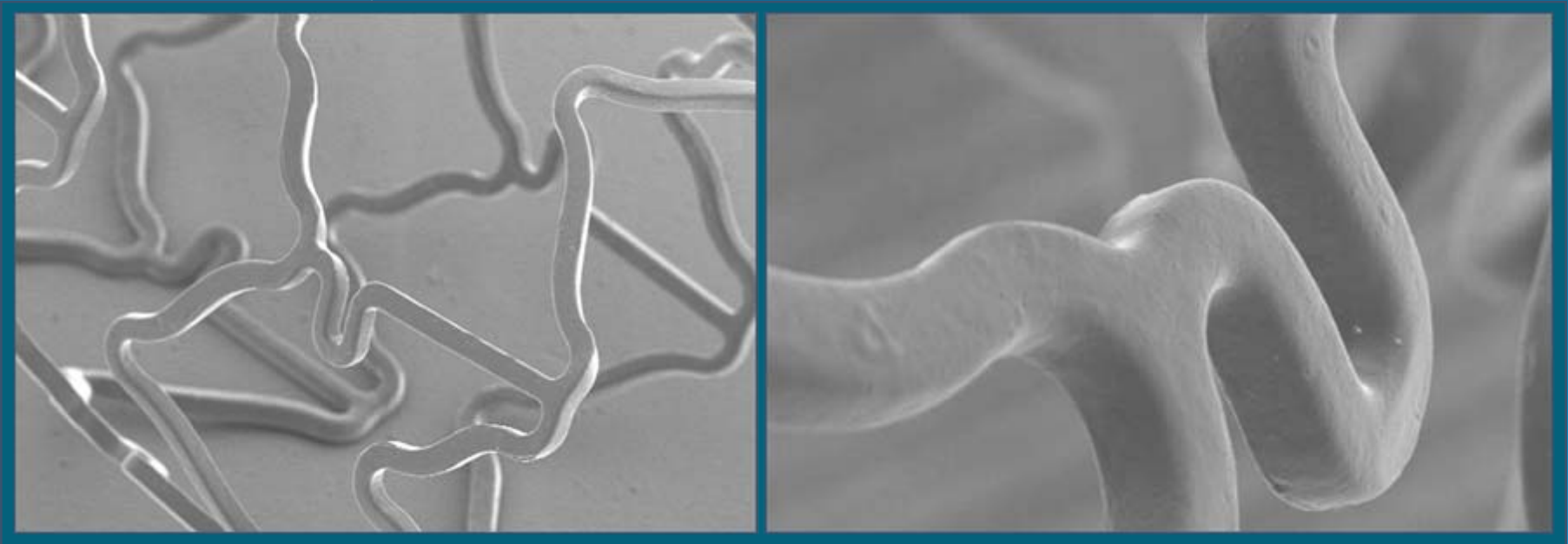


Durable
Fluorinated
Copolymer

ML VISION®
Stent Delivery
System

SPIRIT
Clinical Trials

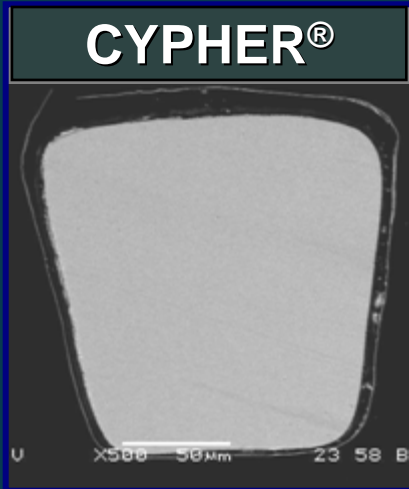
Coating Integrity – XIENCE™ V Fluoropolymer (7.8 um thick)



- Uniform, consistent coating integrity upon deployment
- Good adhesion to stent – no bonding, webbing, tearing
- Non-tacky drug matrix prevents “unwanted” adhesions

DES Strut and Polymer Thickness

3.0 mm diameter stents, 500x magnification



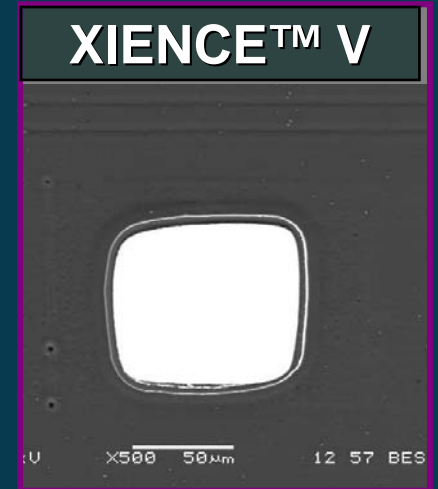
Strut Thickness:
140 µm
Polymer Thickness:
12.6 µm
Total:
165.2 µm



Strut Thickness:
132 µm
Polymer Thickness:
16 µm
Total:
164 µm



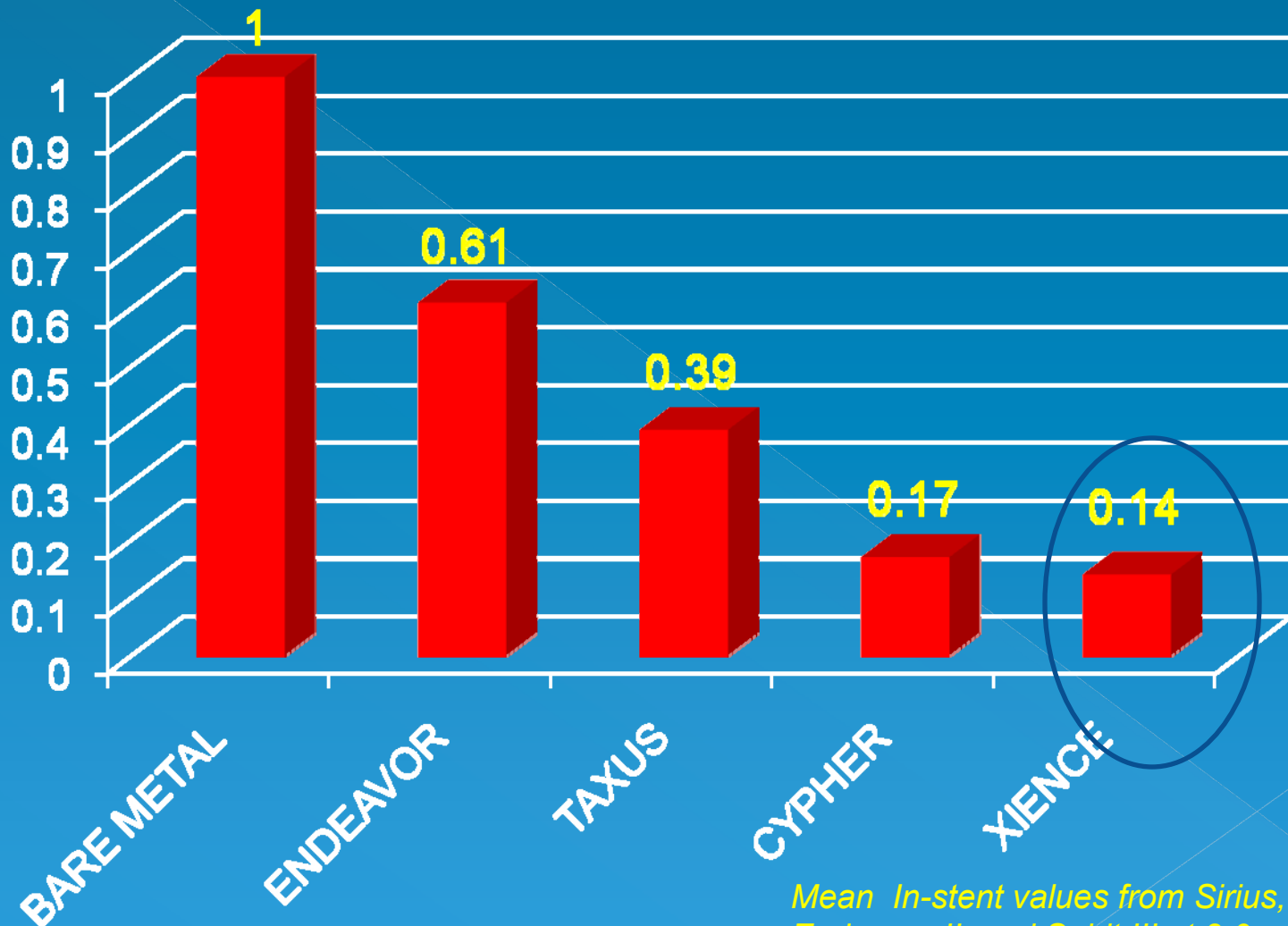
Strut Thickness:
91 µm
Polymer Thickness:
5.3 µm
Total:
101.6 µm



Strut Thickness:
81 µm
Polymer Thickness:
7.8 µm
Total:
96.6 µm

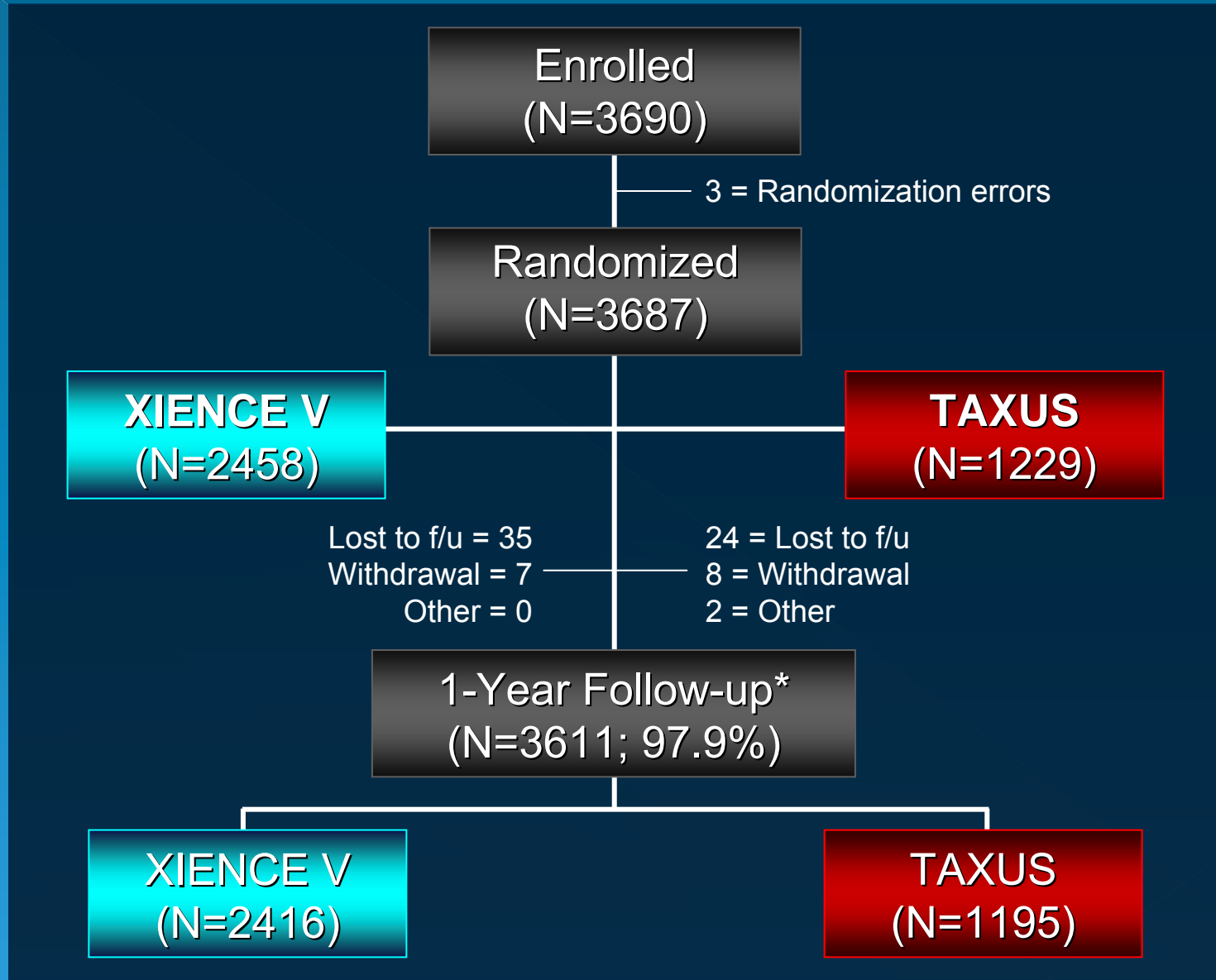
Late Loss* (mm)

An (imperfect) Index of Anti-restenotic Efficacy



Mean In-stent values from Sirius, Taxus IV Endeavor II, and Spirit III at 8-9 months

SPIRIT IV Study Protocol

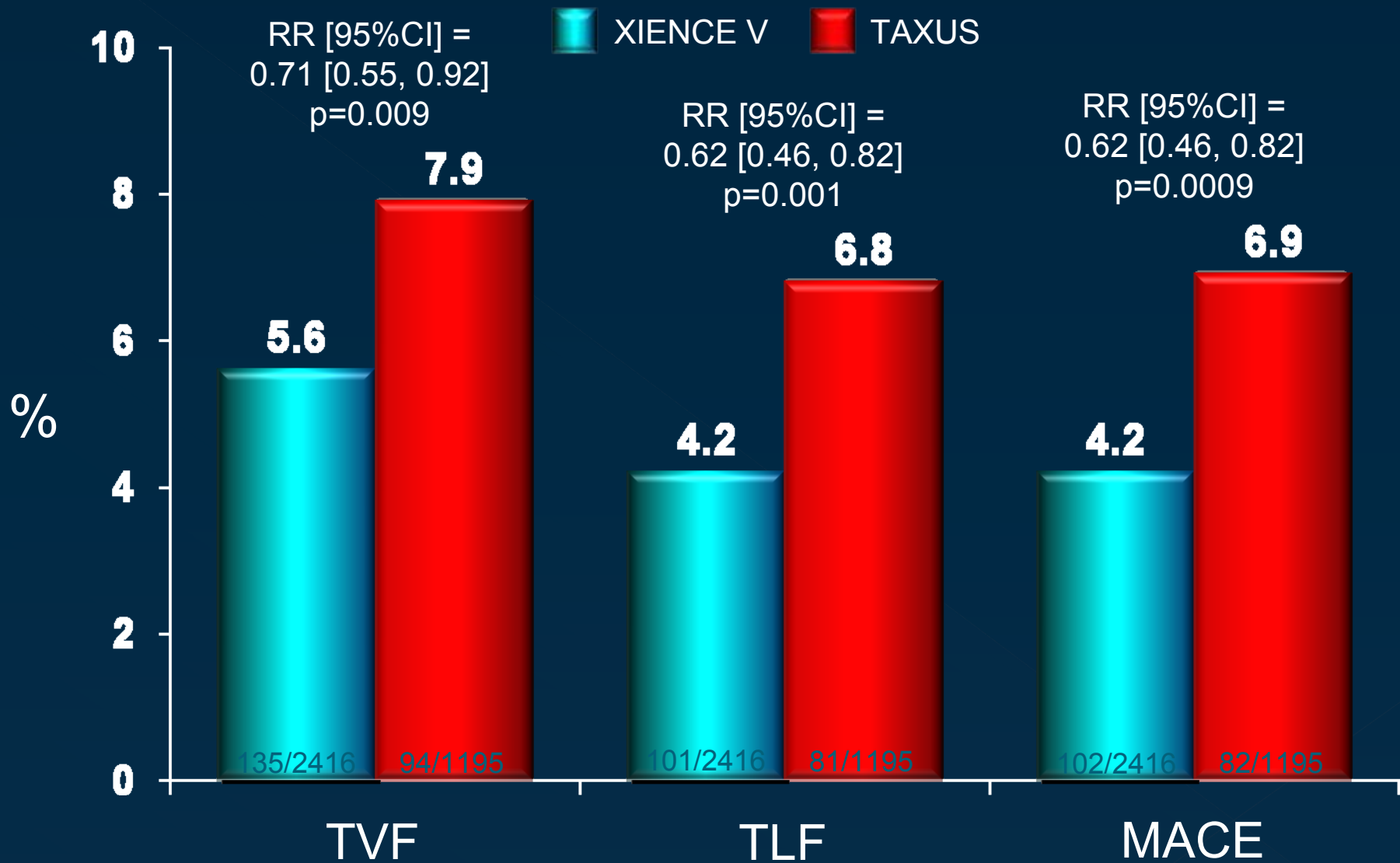


*F/U window: \pm 28 days

TCT 2009

Spirit IV

TVF, TLF, and MACE Through 1 Year

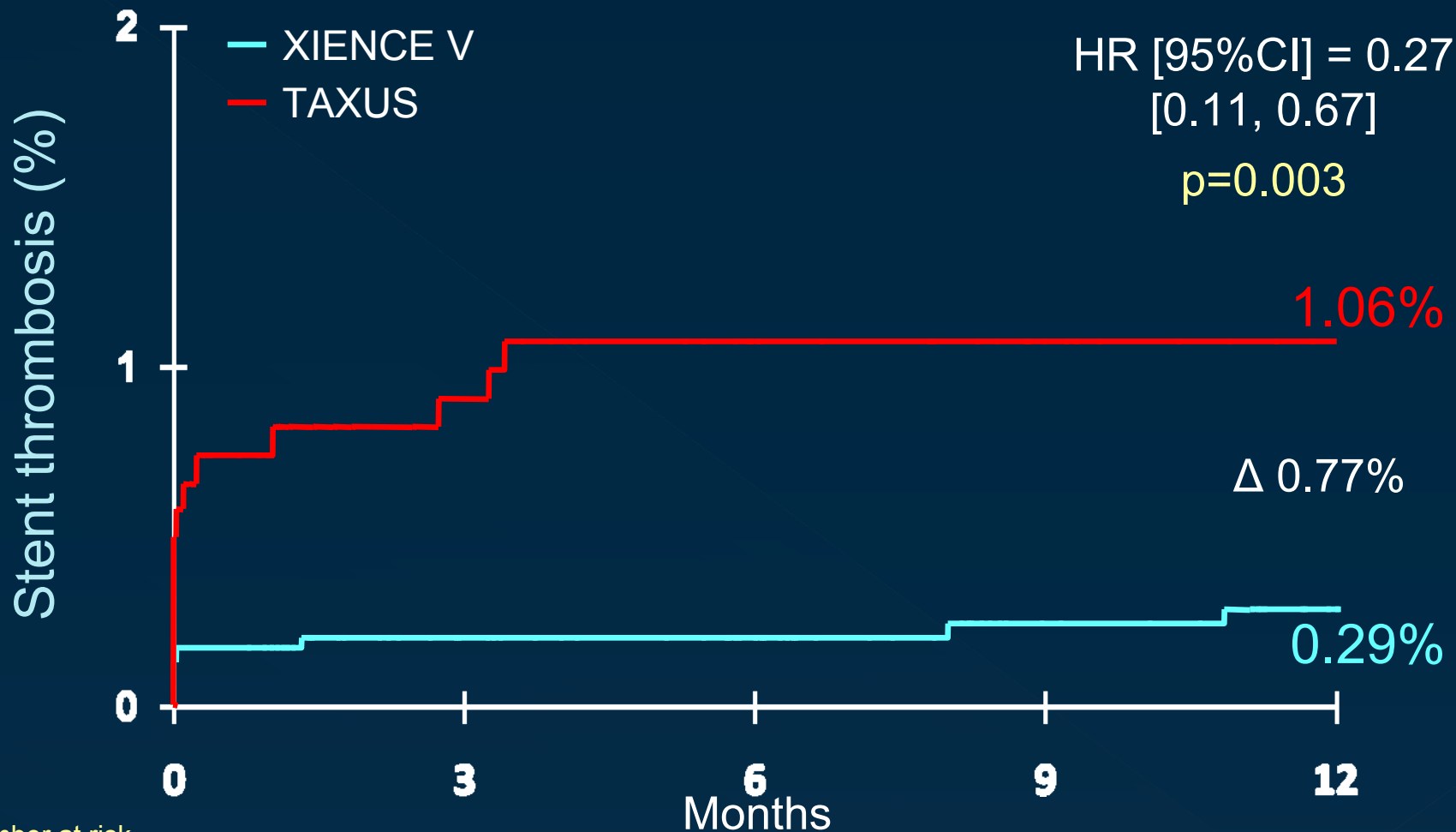


TLF = cardiac death, target vessel MI, or ID-TLR; MACE = cardiac death, all MI, or ID-TLR; TVF = cardiac death, all MI, or ID-TVR. 1 Year = 365 ± 28 days

TCT 2009

Spirit IV

Stent Thrombosis (ARC Def or Prob)

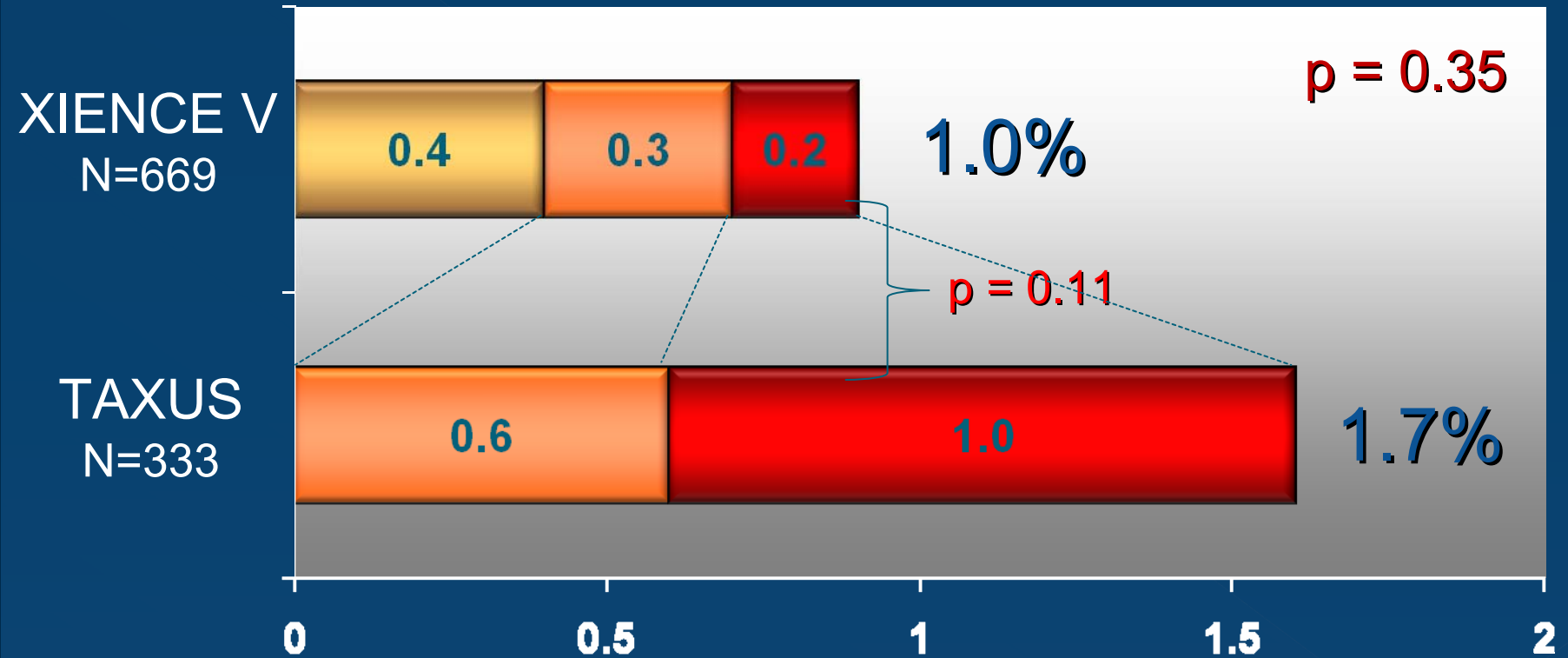


Number at risk

XIENCE V	2458	2426	2412	2388	2376
TAXUS	1229	1195	1184	1174	1166

Stent Thrombosis (Protocol Definition)*

■ Early (0 – 30 days) ■ Late (31 days – 1 year*) ■ Very Late (1 – 3 year*)



Stent thrombosis (%)

Spirit III

*ACS + angiographic thrombus, or unexplained death or STEMI/Q-wave MI in target lesion distribution within 30 days

*Includes F/U window of ± 28 days

XIENCE PRIME : Next generation workhorse everolimus-eluting stent



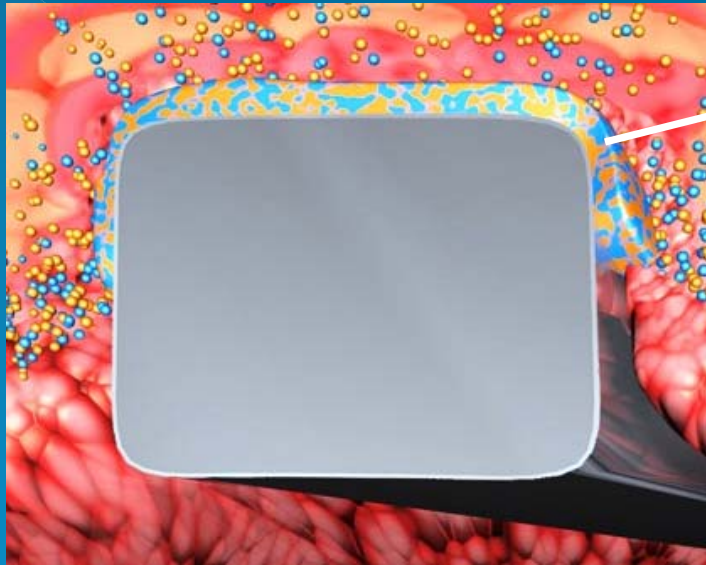
New SDS Enhanced stent

- More flexible and deliverable
- Higher RBP
- Shorter balloon tapers

OTHER DES PLATFORMS

- NOBORI BIOLIMUS
- BIOMATRIX BIOLIMUS

BioMatrix Biolimus-Eluting Stent



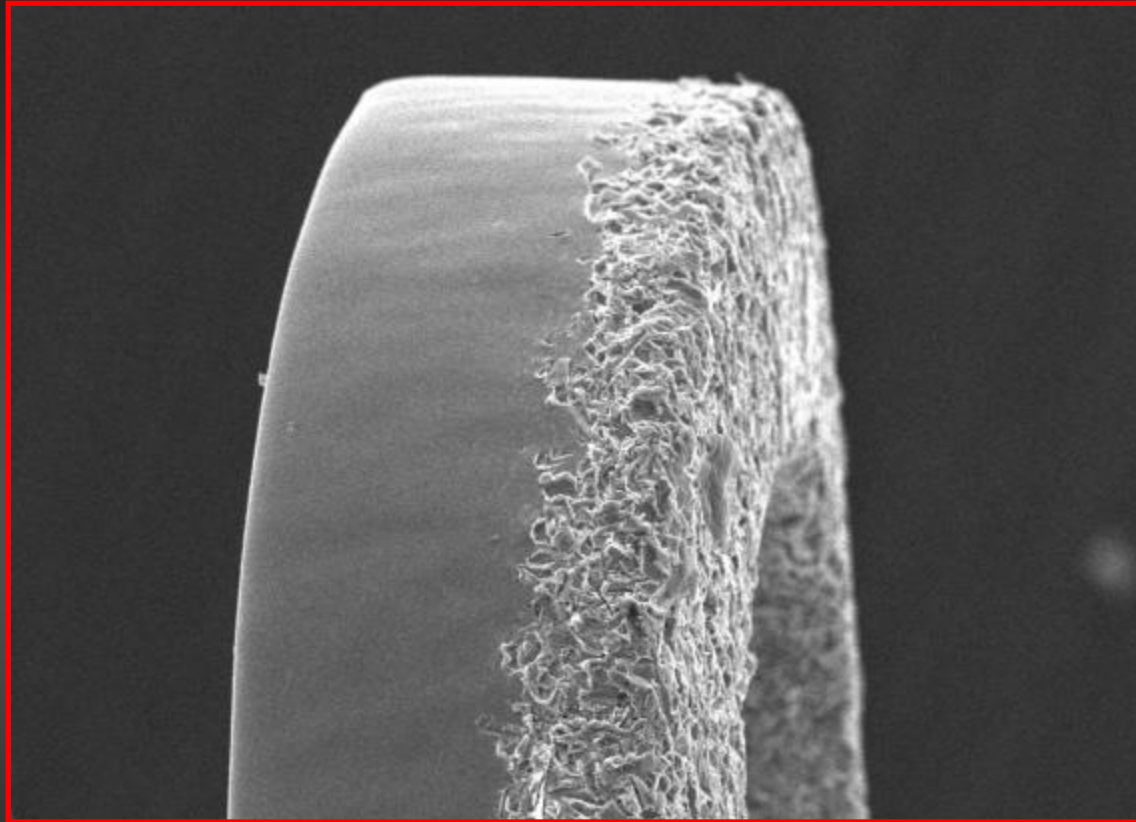
Biolimus (Sirolimus derivative) and PLA Biodegradable Polymer in Abluminal Stent Surface



Stainless steel stent platform has a strut thickness of 112 μm

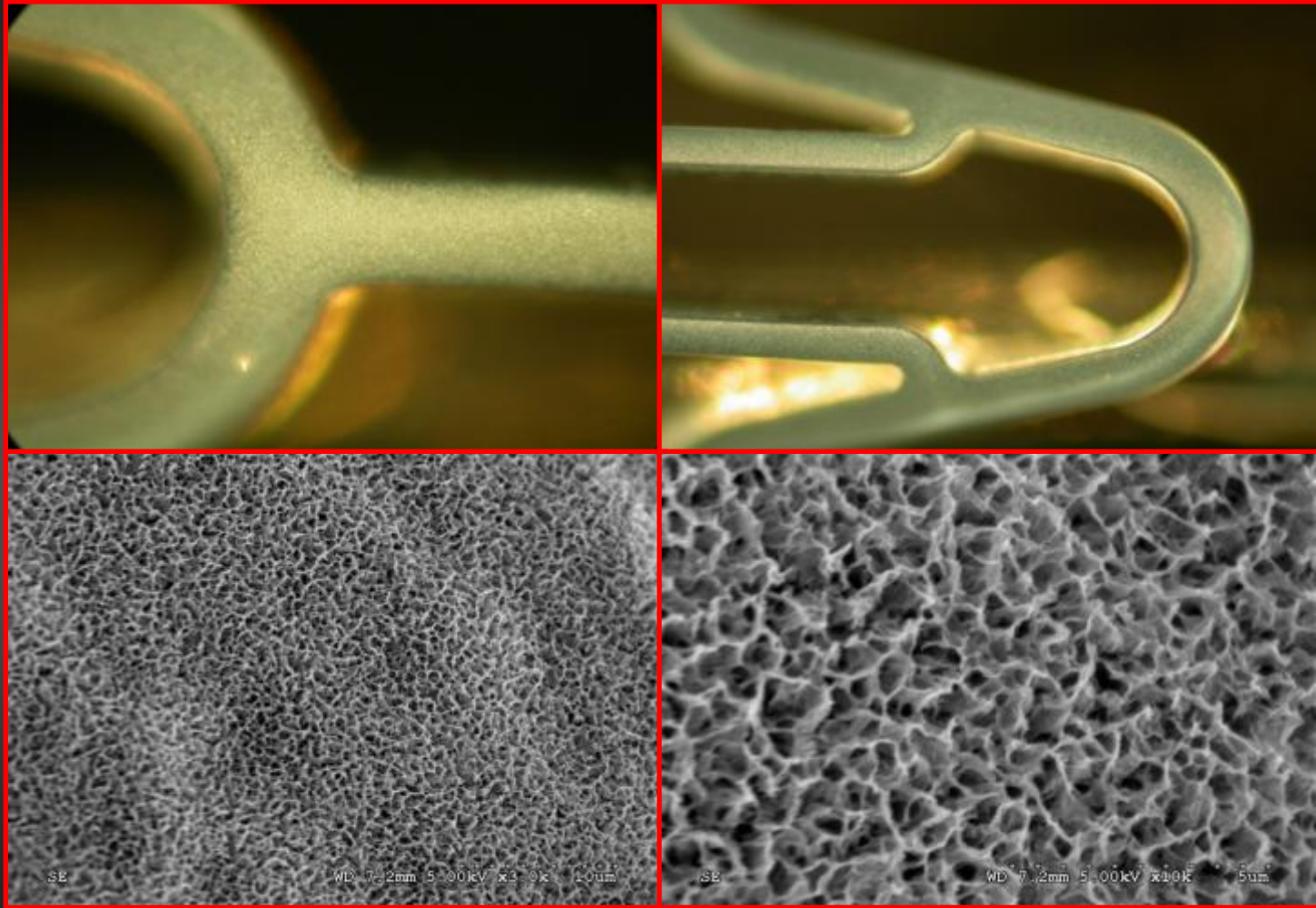
BioMatrix Freedom Stent

Micro-structured Surface



- **Selectively micro-structured surface holds drug in abluminal surface structures**

3D MicroPorous Nanofilm HAp



Dedicated Bifurcation Stents



AST petal



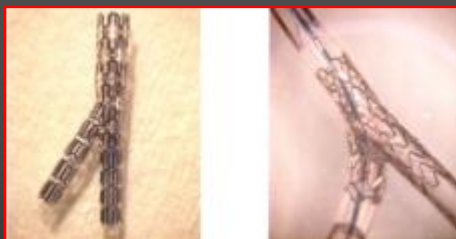
Guidant frontier



Trireme



Devax (+ BA9)



"true" bifurcation designs



sidebranch designs



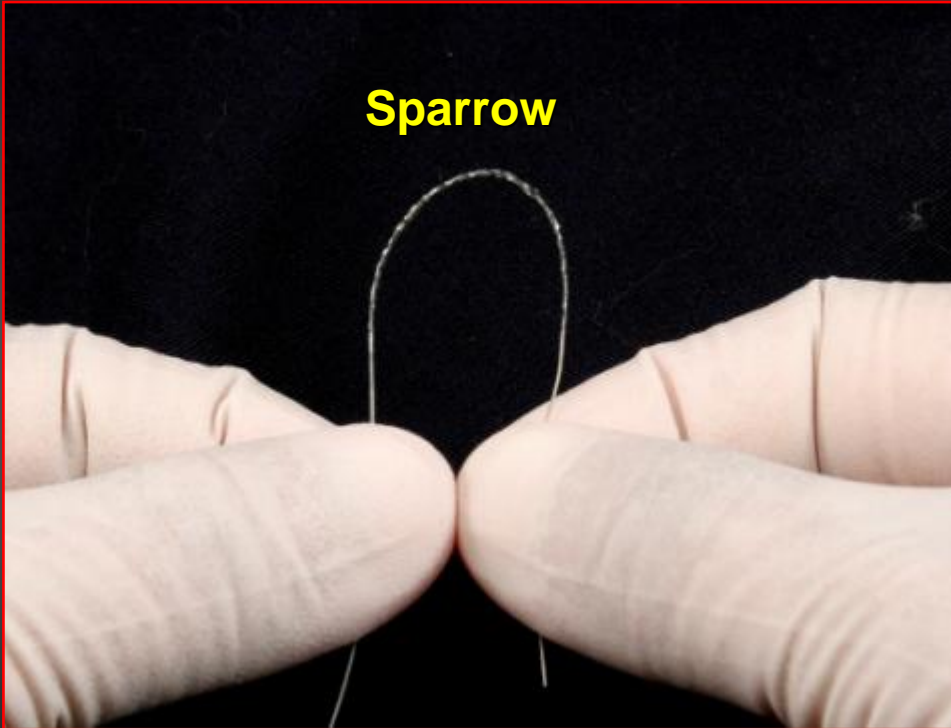
MGuard Stent

A stent wrapped with ultra-thin polymer mesh sleeve, knitted to the external surface



The CardioMind Sparrow™: Stent on a .014" Guide Wire Platform

Sparrow

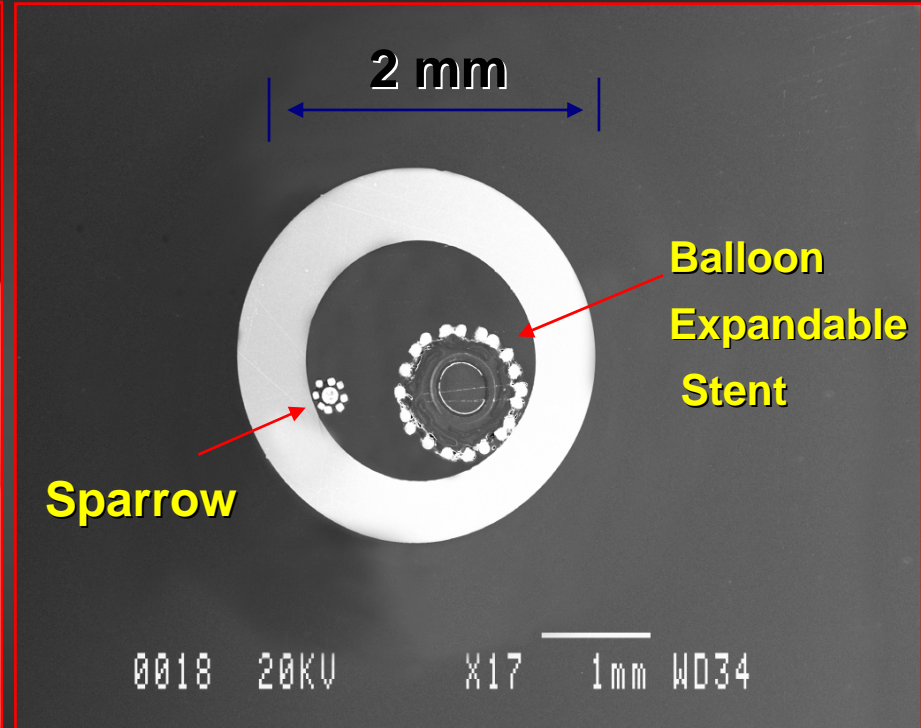


2 mm

Sparrow

Balloon
Expandable
Stent

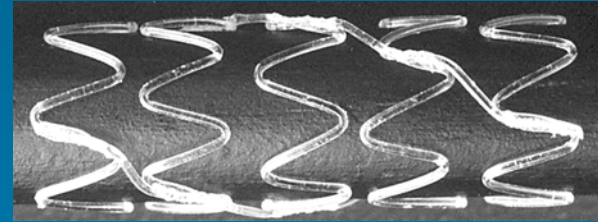
0018 20KV X17 1mm WD34



Bioabsorbable Stents

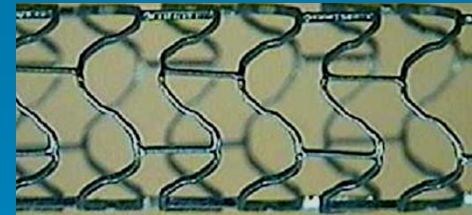
- ▶ Igaki-Tami (Igaki Medica Planning Co Ltd)
- ▶ Magnesium (Biotronik)
- ▶ REVA (REVA Medical)
- ▶ BTI (Bioabsorbable Therapeutics Inc)
- ▶ BVS (Abbott Vascular)

Igaki-Tamai stent

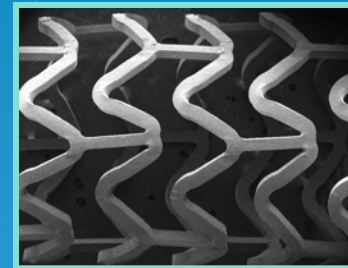


PLLA

Bioabsorbable Magnesium Stent



BVS (Abbott)



PLLA and
PDLLA
Everolimus

How about DRUG
ELUTING BALLOONS
(no stent or provisional
stenting)?

Local Drug Delivery: Paaccocath-DEB vs. DES

Drug-Eluting Balloon

Immediate release
Short-lasting exposure
~ 300 - 600 μg dose
No polymers
Wiped off the balloon surface
Premounted stent optional

Drug-Eluting Stent

Slow release
Persistent drug exposure
~ 100 - 200 μg dose
Polymer
Diffusion from stent struts
Stent mandatory



- Conventional angioplasty balloon catheters
- Coated with paclitaxel
(+ contrast medium as matrix builder and release supporting additive)
- Controlled dose, homogeneity of coating, non-toxic excipients

PACCOCATH[®]-Technology: The Matrix Coating of SeQuent[®] Please

Pure paclitaxel



matrix coating:

paclitaxel + hydrophilic spacer

(iopromide = Ultravist[®])



The hydrophilic spacer leads to:

- Porous coating with a high contact surface between the lipophilic drug molecules and the vessel wall
- Uniform and complete release of the target drug dose after first balloon expansion that guarantees:
- A high bioavailability of paclitaxel on the target side for rapid drug absorption by the vessel wall

PEPCAD II ISR - Outcome, 6 months FU

n=126

	SeQuent Please	Taxus	p
n	66	60	
Follow-up	6.2 ± 0.8	6.2 ± 0.8	0.7
Control angiography	58 (87.9 %)	54 (90.0 %)	0.8
Late lumen loss	0.19 ± 0.38	0.47 ± 0.71	0.03
Binary restenosis in segment	2 / 58 (3.4 %)	11 / 54 (20.4 %)	0.007
TLR	2 / 64 (3.1 %)	10 / 60 (16.7 %)	0.02
Myocardial infarction	0 / 64 (0.0 %)	1 / 60 (1.7 %) <small>NSTEMI due to side branch occlusion</small>	1
Death	2 / 64 (3.1 %) <small>1 non-cardiac, 1 cardiac but not lesion related</small>	1 / 60 (1.7 %) <small>non-cardiac death</small>	1
MACE (w / o noncardiac death)	3 / 64 (4.7 %)	11 / 60 (18.3 %)	0.02

Much more to
come...

Thanks

